

NOKIA MOBILE PHONES

December 30th, 1998

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FEDERAL COMMUNICATIONS COMMISSION
Equipment Authorization Branch
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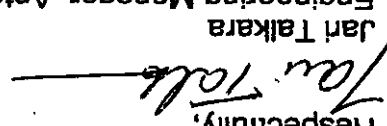
SAR TEST REPORT of Nokia 5180

Gentlemen,

Please find attached SAR test report of FCC ID: GMLNSD-1GX

For and on behalf of Nokia Mobile Phones Ltd.

Respectfully,


Jari Talkara

Engineering Manager, Antennas

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1. Description of the measurement

This measurement was done by E-field scanning system for dosimetric assessments. It is robot-based system which allows automated E-field scanning in tissue simulating solutions. The measurements are based on the induced specific absorption rate (SAR) definition of relevant ANSI / IEEE standards. The dosimetric assessment system of Nokia Mobile Phones is manufactured by Prof. Niels Kuster at ETH (Schmid & Partner Engineering AG) in Switzerland, Europe.

The method used to determine the 1gram average value of SAR is:

Initially a coarse scan is performed over the whole area on a 15 x 15 mm grid. From this coarse scan, the location at which the maximum value is measured is used as the centre for a second, more detailed scan. This second scan is based on a 3 dimensional grid of 4 x 4 x 7 points on a grid of 10 mm. The average SAR values are computed using the 3D spline interpolation algorithm. The 3D spline is composed on three one-dimensional splines with the "Not a knot" condition in the x, y and z directions (1), (2). The volume is integrated with the trapezoidal algorithm. 1000 points (10x10x10) are interpolated to calculate the average. All neighbouring volumes are evaluated until no neighbouring volume with a higher average is found.

(1) W. Gander, *Computermathematik*, Birkhauser, Basel, 1992

(2) W. H. Press, S. A. Teukolsky, W. T. Vetterling and B. P. Flannery, *Numerical Recipes in C, The Art of Scientific Computing*, second edition, Cambridge University Press, 1992

2. Description of calibration by manufacturer

The calibration of data acquisition electronics and probe was done by the manufacturer. (Appendix 3 and 7)

- the data acquisition unit is calibrated and tested using a FLUKE 702 Process Calibrator

- measurement uncertainty is less than $\pm 20\%$ for various tissues simulating solutions and frequencies:

- these calibration parameters were measured using a temperature probe developed by manufacturer
- description of the probe calibration and examples of the evaluation are enclosed in Appendix 7

3. List of standards

IEEE Std C95.1-1992

IEEE Standard for Safety Levels with Respect to Human Exposure to Radio Frequency Electromagnetic Fields, 3 kHz to 300 GHz

IEEE Std C95.3-1992

IEEE Recommended Practice for the Measurement of Potentially Hazardous Electromagnetic Fields-RF and Microwave

4. Device list:

- Automated E-field scanning system for dosimetric assessments System.
Calibration due August 1999. Technical data (Appendix 1)
- Probe ET3DV4, SN: 1105, Recalibrated due August 1999
Technical data (Appendix 2)
- DASY-dosimetric assessment system, DAE V2, SN: 213, Calibration
due August 1999 (Appendix 3)
- Industrial robot and Control unit, type STÄUBLI CS7 RX 90(CR)
NO:595148-01, Technical data (Appendix 4)
- Generic Twin Phantom Version 3 (Appendix 6).
- PC COMPAQ 466
laser printer QMS magicolor plus
- Devices for preparation of the brain tissue simulating liquids
-General laboratory equipment for preparation of liquids
-Magnetic stirrer with heating plate IKA RET CV, SN:792708
-Scale Mettler Doletto, SN: 2114177678
- HP 85070A Dielectric probe system
- network analyzer HP 8753B, SN:2716U00762, Calibration due April 1999
- cables
- probe stand
- dielectric probe kit NO: US33020242
- PC AST PREMMIA 4/66 d
- HP-IB 82335B (interface and software)
- Dipole Validation kit, Schmid & Partner Engineering AG, Typ: D900V2, SN:
003, Recalibrated/Verification due August 1999
- signal generator ROHDE & SCHWARZ, 1038.6002.03 , Calibration due
July 2000
- power meter, ROHDE & SCHWARZ, 857.8008.02, Calibration due
November 1999
- amplifier ZHL-42 (SMA), 022488-RM:4152

5. Equipment under test

Unit: NOKIA 5180
 FCC-ID: GMLNSD-1GX
 SN: 32204

5.1 Verification and results

Validation of the measurement system was made before measurement using the Validation kit. Appendix: 8 and 9

This validation measurement makes sure that the repeatability of SAR measurement value with careful positioning is better than 10 %.

The error was < 2 % compared to the parameter of manufacturer SAR results (0.25W): 2.34 mW/g (1g) and 2.38 mW/g (1g). Appendix: 8 and 9

5.2 Specification of Liquid

The liquids was done using the "Recipe 900MHz " for liquid of brain tissue at 900 MHz, respectively, and preparation bases on brochure. Appendix 5

900 MHz liquid was used with the probe validation kit measurement.

The parameters was measured by liquid testing of HP85070A Dielectric probe system.

The amounts of used liquids were 20 litres.

Liquid parameters ϵ_r (Relative permittivity) and σ (Conductivity) were measured by HP 85070A Dielectric probe system.

900 MHz:	$\epsilon_r = 41.3$	$\sigma = 0.86$
824 MHz:	$\epsilon_r = 42.1$	$\sigma = 0.79$
836 MHz:	$\epsilon_r = 41.9$	$\sigma = 0.80$
849 MHz:	$\epsilon_r = 41.8$	$\sigma = 0.81$

5.3 Specification of position with phone against generic twin phantom

The position of the phone relative to the head phantom is shown on page 8. The centre of the phone's earpiece is aligned such that it is co-axial with a mark on the phantom which represents the centre of the ear on the left side of the head.

Measurement was done with a Left-Hand (L.H.) side because the helix phone antenna is situated in the top right corner of the phone (viewed from the earpiece side). Therefore, the antenna is closer to the head in the measurement position using a L.H. side rather than a R.H. side. It is concluded that the L.H. side is worst case measurement position.

The test signal for SAR measurement was analog AMPS.

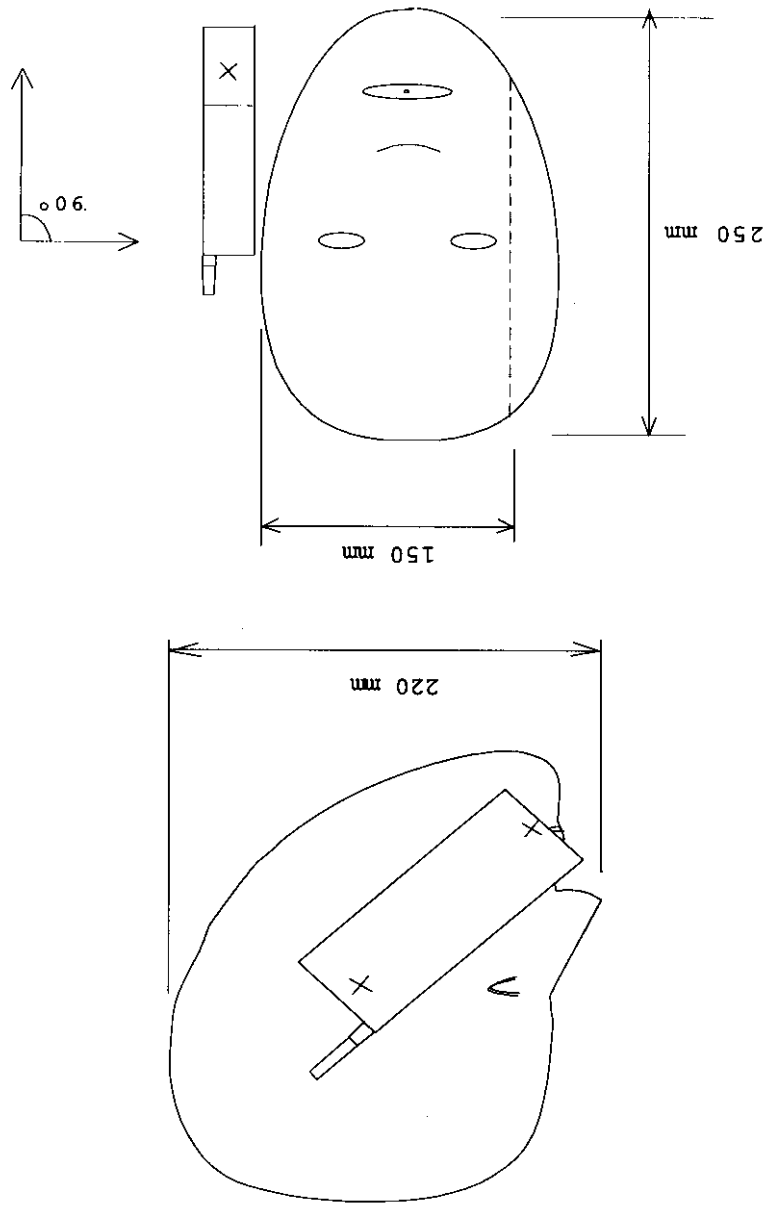
The phone position against the head was in Normal phone position (for the IEEE Std C95.1-1992 (ANSI / IEEE) and FCC measurement). The angle between the reference line of the phone and the line connecting both auditory canal opening was 90°. The distance between the handset and the ear area of phantom head is 4 mm (page 8). Measurements of the phone were done with fixed helix antenna.

The used radio channels were: 991, 383 and 799.

TX power of analog AMPS test signal ("Power" in the table of the paragraph 5.5) was measured from external antenna connector of the transceiver using power level 2. During the tests the battery was fully charged.

Ambient and "brain tissue" liquid temperature was 23 °C $\pm$ 1 °C.

5.4 The phone position against generic twin phantom



5.5 Results of SAR for 1g. Appendix: 10

The plots in Appendix 10 are a graphical representation of the SAR values over the whole area being scanned.

Appendix 10, page 4 (nr:4), has sketch of the phone added on the plot for clarifying the position of the phone with respect to the measured SAR values. The size of the area being scanned is sufficiently large to ensure that all possible regions of peak SAR are measured. This is indicated by the fact that the position of peak SAR is in the measured area, and the value of SAR reduces asymptotically in the x- and y- directions as the probe is moved towards the border of the measured area.

Analog mode AMPS

meas nr:		Phone position	Frequency MHz / channel	Power [dbm]	SAR (1g) [mW/g]
1		90°	824.0 / 991	25.1	0.92
2		90°	836.0 / 383	25.2	1.28
3		90°	849.0 / 799	25.5	1.09
FCC ID: GMLNSD-1GX			FCC limit		1.60 [mW/g] (ANSI/IEEE)
MEASURED: 17.12.1998 / NMP					

See Table

NOKIA

07 Jan 99

NOKIA MOBILE PHONES INC.
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Federal Communications Commission,
Authorisation & Evaluation Division,
7435 Oakland Mills Road,
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Attention: Equipment Authorisation Branch

Addendum to the SAR report of 5180

Output power levels of Nokia 5180 are measured in production as well as in all testing cases at the external antenna connector and are set to be within the limits of the attached tuning document.

In the attached SAR TEST REPORT only the AMPS-mode is measured. In 800MHz CDMA mode the SAR values are much lower due to the 1.0dB lower output power. In another product Nokia 6185 (FCCID: GMLNSD-3AX) the measured max. SAR values were 1.53mW/g in AMPS mode ($P_o=25.5\text{dBm}$) and 1.07mW/g in CDMA mode ($P_o=24.0\text{dBm}$). Nokia 5180 is basically the same phone as 6185 but without 1900MHz CDMA mode and 5180 is also thicker lowering the SAR values further.

NOKIA MOBILE PHONES INC.

Jari Niemela

Product Project Manager, Product Development, San Diego

Appendix 1

pages 1 - 9

AUTOMATED E-FIELD SCANNING SYSTEM FOR
DOSIMETRIC ASSESSMENTS

Automated E-Field Scanning System for Dosimetric Assessments

Thomas Schmid, Oliver Egger and Nils Kuster

Swiss Federal Institute of Technology
Zurich, Switzerland

Abstract—The interest in accurate dosimetric measurements inside phantoms that simulate biological bodies has burgeoned since several regulatory commissions began calling for or recommending the testing for compliance with safety standards of low power devices. This paper presents a newly developed, robot-based system that allows automated E-field scanning in tissue simulating solutions. The distinguishing characteristics of the system are its high sensitivity and its broad dynamic range ($1 \mu\text{W/g}$ to 100 mW/g) over the entire frequency range (10 MHz to over 3 GHz) used for mobile communications. The reproducibility of the dosimetric evaluations has been shown to be considerably better than $\pm 5\%$. This has been accomplished by the use of an improved isotropic E-field probe connected to amplifiers with extremely low noise and drift characteristics in conjunction with digital processing of the data. Special emphasis has been placed on system reliability, user-friendliness and graphic visualization of data.

Keywords—

1. INTRODUCTION

The question of whether low power transceivers comply with current safety limits was first raised by Cleveland et al. [1]. Two years later the study of the absorption mechanism in the near field of sources revealed a direct contradiction of the exclusion clause for low power devices with basic safety restrictions [2]. Additional findings of the latter study relevant for this paper were:

- In the close near field, induced currents are mainly caused by the inductive coupling of the high frequency (HF) current distribution on the radiating structure with the biological body.
- The induced specific absorption rate (SAR) depends more on the actual design and the position of the radiating structure with respect to the body than on the inhomogeneity of the tissue.
- Devices with an input power of considerably less than 1 W might violate the basic safety limits for partial body exposure which are: 1.6 mW/g averaged over 1 g (ANSI/IEEE [3]), 2.0 mW/g averaged over 10 g tissue (CENELEC [4]) respectively.

These findings have been confirmed in the following by studies with partially homogeneous bodies exposed to dipole and helix antennas [5], [6] and by a study with largely inhomogeneous head phantoms [7]. Several recently published dosimetric studies on current mobile phones found spatial peak SAR values in the range

Author's address: Swiss Federal Institute of Technology (ETH), CH-8093 Zurich, Switzerland – Submitted to IEEE Transactions on Microwave Technology, January 1995, Accepted in July 1995

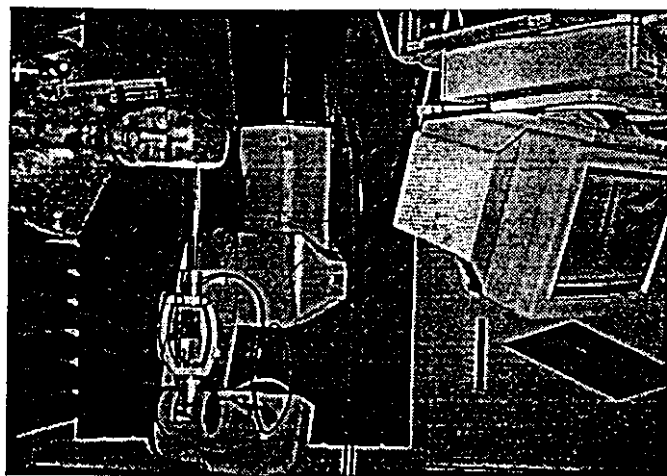
of the safety limits for uncontrolled environments [8], [9], [10], [11], [12], [13]. Under certain conditions, these limits were exceeded [8], [11], [10], [13]. This caused some concern in the industry as the current trend towards miniaturization with shorter antennas is bound to lead to higher absorption if these issues are not carefully considered during the design process.

Taking various concerns and factors into consideration, individual type approval using dosimetric tests is the most sound approach for both the public as well as industry. As far back as 1992, the German Agency for Radiation Protection [14] recommended type approval for mobile communication devices. The FCC [15] has now taken a similar stance and is calling for the demonstration that the maximum SAR for PCS devices with output power of more than 100 mW complies with the ANSI/IEEE guidelines for SAR values.

Needless to say, such test procedures will lead to decisions with far-reaching economic consequences. It is therefore essential that the testing procedure meets the highest possible standards of accuracy, reproducibility, standardization and availability during the design procedure of new devices. A critical issue is the operating position of the device being tested. In case compliance must be demonstrated for the use of the device under all operational conditions [14], it is not sufficient to test the device by measurement or computation in one particular predefined position (e.g., normal position). Instead, the "worst case" exposure situation among all operational conditions must be tested. This "worst case" exposure situation can only be determined by varying the most relevant parameters such as the position of the device, the operational condition of the device (e.g., extended or retracted antenna), use by left or right handers, variations of head shape and the position of the hand holding the device.

As no system is yet available that satisfies all these requirements, several groups are currently engaged in developing numerical simulation tools or measurement systems for safety assessments of handheld transceivers. Although anatomical details can now be represented with considerable detail, the numerical approach is fraught with serious difficulties: (1) As today's transceivers have been optimized with regard to size, weight and appearance, simple modelling of the transmitter as a metal box with antenna may not suffice, even if the geometry has been correctly discretized. The reason is that consideration of HF currents may flow on internal substructures of the

Fig. 1. Laboratory set up including robot, probe, data acquisition electronics, phantom and PC.



The HF coupling mechanisms of these internal structures are often not obvious and it can therefore be difficult to arrive at the appropriate numerical modelling. In addition, these effects can undergo considerable changes in the vicinity of the scatterer. (2) If compliance under all operational conditions is required, a number of simulations must be performed, which necessitate techniques that are efficient, largely independent of the grid orientations and which possess self-validating capabilities. (3) It may also be necessary to show that compliance is achieved despite manufacturing variations.

In contrast, an accurate and highly sensitive measurement set up would allow tests of randomly selected samples of a product whereas no modelling or alteration of the product being investigated would be necessary. The position of the device would be easily modified when seeking the worst case conditions. An important difference to numerical simulations is that only the system (including phantom) and not each measurement must be validated. As the location of the strongly local maximum is not known a priori, the SAR distribution in a larger volume of the exposed tissue must be scanned, requiring a large degree of mobility of the probe within the tissue. This in turn, restricts the possible complexity of the phantom.

This paper presents a system that enables the automated measurement of the absorption distribution as well as the assessment of the spatial peak SAR values inside any tissue simulating solution.

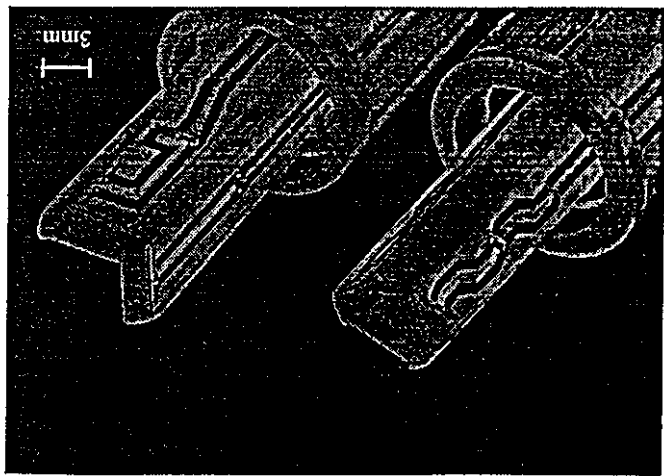
II. LABORATORY SET UP

The SAR can be determined by measuring either the electric field (E) or the temperature rise ($\partial T/\partial t$) inside the exposed tissue.

$$SAR = \frac{\sigma}{\rho} E^2 = c \frac{\partial T}{\partial t} \quad (1)$$

where σ is the conductivity, ρ the density and c the specific thermal constant of the tissue at the site of measurement.

Fig. 2. Tips of the "triangular" (left) and the "rectangular" (right) probes. The tip shell has been removed.



In the set up shown in Figure 1, the SAR distribution is determined by measuring the electric field with miniaturized E-Field probes. Measuring the temperature rise in the simulated tissue does not provide sufficient sensitivity for compliance testing of consumer products [11]. However, this technique is used for the validation of the system as well as for the calibration of the probes (see section VIII). Measurements are done in shell phantoms filled with tissue simulating solution. In the laboratory three types of shell phantoms are used:

- geometrically simple phantoms for calibration and numerical validation of the system
- simplified body and head phantoms to simulate worst-case conditions of exposure with real devices
- very detailed phantoms to investigate the effects of different tissue layers (skin, living bone, air cavities, etc.), different exposure conditions (device positions, hand effect, spectacle frames, etc.) and to validate the simplified phantoms.

The E-field probes are positioned by a 6-axis precision robot (Stäubli RX90) inside shell phantoms with a working range greater than 0.9 m and with a position repeatability that is better than ± 0.02 mm (at constant temperature). Each probe incorporates an optical surface-detecting system, which permits the accurate positioning of the probe with respect to the phantom's surface. Basically the SAR distribution in any volume can be measured. The currently implemented compliance test involves firstly measuring the SAR on a coarse 3D-grid in a preselected volume. Afterwards a fine 3D-grid around the previously detected maximum is measured. The 1g or 10g-average SAR-values are interpolated from the fine-grid results. The procedure is completely automated and takes less than 15 minutes, which is well within the battery lifetime of standard communication devices.

III. ISOTROPIC E-FIELD PROBES

The most crucial components of the whole system are the E-field probes. The main requirements are:

An important part of most antenna design is to suppress secondary reception modes produced by the connecting lines, constructional asymmetries, etc. In the probes described above there are several possible secondary reception modes. One is produced by normal mode signals coupled into the resistive lines and rectified in the diode. These signals can be reduced by decreasing the spacing between the lines or by filtering techniques. Another mode is produced by common mode signals coupled into the lines and converted at the diode into normal mode signals by asymmetrical loading of the diode halves due to constructional asymmetries (especially when measuring in the immediate proximity of metallic structures). As the source impedances of these modes have high resistive components, they are negligible at higher frequencies where the (mainly capacitive) impedances of the antennas and diode are much

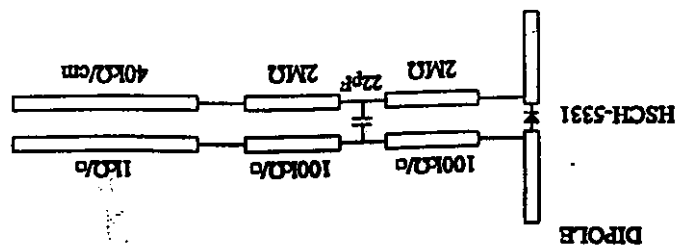
A. Problem 1: Secondary Modes of Reception

been paid to these constructional problems. Improve the directivity of the probes, special attention has been paid to these constructional problems. To further distort the theoretical dipole characteristics. To further supporting materials of the probe, which can completely line), they do not discuss the influence of the dielectric characteristics by modelling the components (dipole-diode (e.g., in [17]). While these papers describe the probe's probe has been discussed previously in various publications lines to the data acquisition unit. The theory of this type of loaded with a schottky diode and connected with resistive Each probe consists of three small dipoles (3mm) directly and a slightly bigger profile.

media [16]. However, the probe has an asymmetric core results in better omnidirectivity, especially in low-epsilon probes, i.e., parallel and normal to the probe axis. This vector components corresponding to the coordinates of the alled to the probe axis enables the separation of the field The "rectangular" design (Figure 2) with one dipole parallel to the probe axis enables the separation of the field of placing the surface detector in the center of the probe. tivity because of the smaller outline and the possibility for dosimetric measurements in liquids with high permittivity. The design with the triangular core (Figure 2) was selected. For optimal performance under different measuring conditions, two types of E-field probes have been developed.

- high sensitivity and linear response over a broad frequency range
- high spatial resolution
- isotropy in differing media
- low interaction with the measured field
- small in size

Fig. 3. Equivalent circuit representation of the probe.



The high resistive decoupling of the diode from the detector circuit has another desired effect. The diode impedance could be significantly reduced by this new approach.

Apparent, the performance degradation caused by direct coupling effects between dipole and line (TEM cell in [10]) diagram of the well known E-field probe in thin film technology (50 μm line spacing and width) described in [17]. For comparison, Figure 5 shows the same axis of the "triangular" probe is shown between 10 MHz and 800 MHz. In Figure 4 the directivity diagram normal to the probe much coarser than those of thin-film probes.

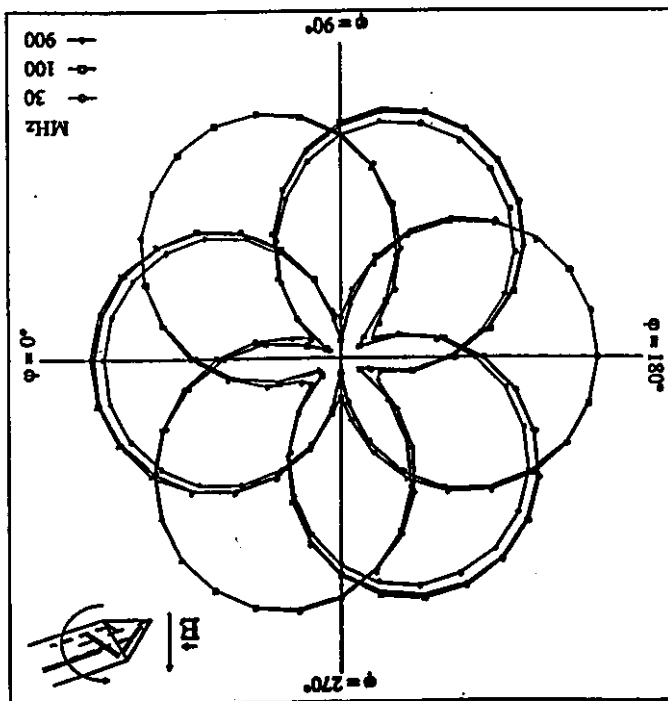
layers are printed using silk screening, the structures are curable with the thin-film technique. Since the thick film production of much higher sheet resistances than manual different sheet resistances on the same substrate, and the thin-film technique. This permits the use of lines with tion of the dipole and lines instead of the normally used The thick-film technique was employed for the construction (see Figure 3).

was introduced between the dipole and the resistive line useful for frequencies down to 10 MHz, a distributed filter In order to suppress these modes and make the probe tivity.

has proven to be of great importance for high probe sensitivity. A carefully designed laboratory grounding system ELP fields produced by power lines or robot control signals. can also be the source of such secondary signals, especially Other electromagnetic fields present in the laboratory tics (see Figure 5).

come dominant and distort the ideal antenna characteristics. At lower frequencies, however, these modes can be-

Fig. 4. Directivity diagram of the new probe in thick-film technique with the E-field normal to the probe axis. Measured using the TEM cell (in [10]) between 10 MHz and 900 MHz.



Any dielectric material around electric dipoles will have an effect on the local signal strength. It is obvious from the construction of these probes that the influence on E-field components normal to the probe axis will be different from those on E-field components parallel to the probe axis. Furthermore, this difference in sensitivity depends on the surrounding media. This results in poor isotropy in planes that include the probe axis.

Figures 6 and 7 show the deviation from isotropy of the probe with triangular design in air and brain simulating solution in a plane normal to the probe axis and in a plane through the probe axis, respectively.

B. Problem 2: Influence of the Probe Materials on the Field

Figure 13, the rms response of this approach is tested for duty cycles of up to 100%. This prevents the usual "peak detector characteristic" of diode detector probes for pulsed signals. In

Fig. 6. Deviation from isotropy of the probe with triangular design in air, whereby the E-field was rotated in a plane normal to the probe axis. Measured using the TEM cell (H110) between 10 MHz and 900 MHz and the waveguide R26 at 2500 MHz.

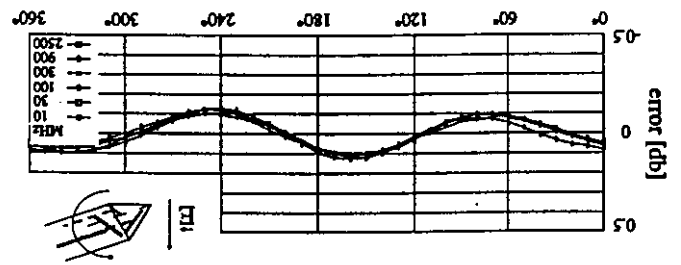
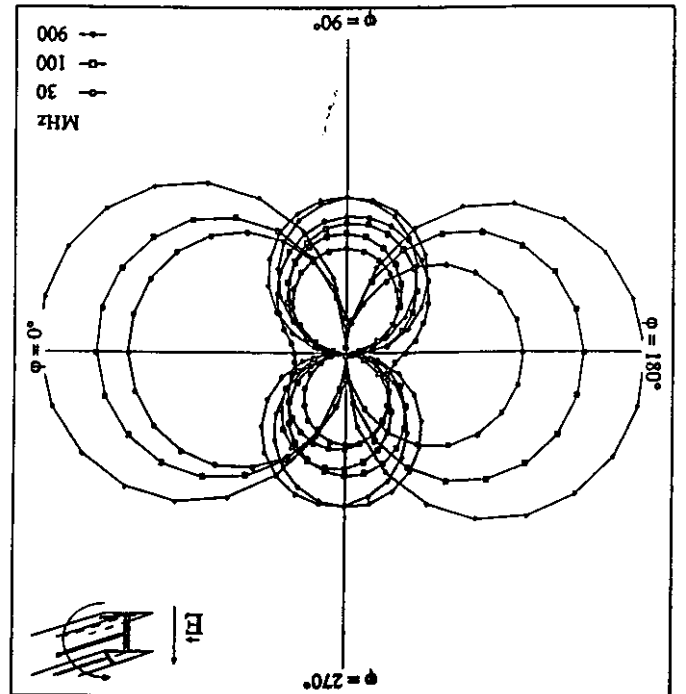


Fig. 5. Directivity diagram of the standard probe in thin-film technique with the E-field normal to the probe's axis. Measured using the TEM cell between 10 MHz and 900 MHz.



The probe with the triangular design was selected for dosimetric measurements for the following reasons:

- There was slightly better isotropy in planes normal to the probe axis due to the high degree of constructional symmetry in this plane.
- The slightly weaker isotropy in the other planes in solutions with high water content is not a significant drawback. The reason being that the components of the E-field along the probe axis, i.e., normal to the phantom surface, have been shown to be significantly smaller than components in other directions. This has

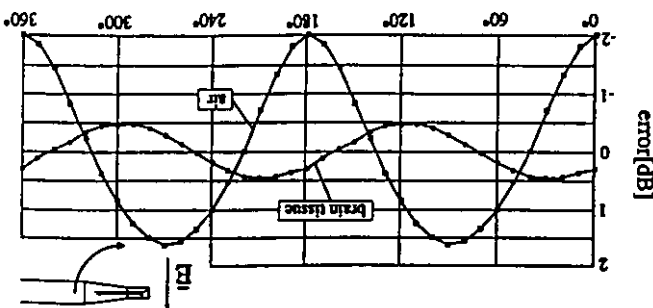
Another approach is to compensate for these effects by numerically weighting the dipole-signal input according to the field orientation with respect to the probe extension. This is only possible if the component of the E-field along the probe axis can be separated, i.e., if one of the probe's dipoles is aligned along the probe axis. This has been successfully accomplished in the "rectangular" design which is described in [16] (see also Figure 2). By simply introducing a media-dependent conversion factor for the signal of the component along the probe axis, the isotropy in air is better than ± 0.5 dB in all directions and for all polarizations.

By selecting material for construction with the same characteristics as the surrounding media. As such material must be easily mechanically processible, no such materials for air or for biological tissue are available. By adjusting the angular orientation of the dipoles in order to compensate for the different sensitivities along and normal to the probe axis. It follows that such a probe would only be usable in a single surrounding media.

This problem can be overcome in the following ways:

- By selecting material for construction with the same characteristics as the surrounding media. As such material must be easily mechanically processible, no such materials for air or for biological tissue are available.
- By adjusting the angular orientation of the dipoles in order to compensate for the different sensitivities along and normal to the probe axis. It follows that such a probe would only be usable in a single surrounding media.

Fig. 7. Deviation from isotropy of the probe with triangular design in air at 2500 MHz (above an open waveguide R26) and in brain tissue equivalent solution (900MHz), whereas the E-field was rotated in a plane through the probe axis.



been predicted in [2] and is demonstrated in Figures 8 and 9. Hence, the maximum error introduced by this lack of isotropy is much less than the deviation of ± 0.6 dB in Figure 7.

- The fact that the dipole orientation differs from the probe orientation is not a disadvantage because only the total field is of interest in dosimetric applications.
- The high degree of constructional symmetry improves the efficiency of the described filtering method for secondary reception modes. The frequency response at frequencies below 100 MHz is better than in the probe with the "rectangular" design.
- The triangular design is very compact and ensures a high spatial resolution. The distance between the dipole centers is less than 2 mm.
- The surface detection system (see Section V) is positioned in the center of the probe. This ensures excellent positioning accuracy even when the probe is not normal to the phantom surface.

C. Problem 3: Influence of the Probe on Inhomogeneous Fields

The disturbance caused by the probe on inhomogeneous fields depends not only on the probe material and geometry but also largely on the field itself. The influence of these effects must be investigated in each case. Figure 14 shows the results of SAR measurements in brain simulating solution near the shell of the phantom.

If the distance between the probe tip and surface of the phantom is less than 1 mm, the field distribution inside the probe tip differs due to short circuiting between the probe and the outside media, i.e., the measured values become too high. This error source is greater than the error caused due to scattering effects by the probe at the interface [18]. The problem can be solved by measuring the SAR at different distances from the surface and extrapolating the SAR values to the surface. (This extrapolation procedure is also necessary because of the separation of the dipole center from the probe tip).

Another source of error in inhomogeneous fields arises from the spacing between the dipole centers in the probe. Because each field component is measured at a slightly different location, discrepancies are to be expected where field magnitudes or directions change rapidly within the probe's dimensions. Because of the nature of the absorption mechanism [2], the field gradients induced by mobile phones operating at frequencies below 3 GHz have larger dimensions than the probe's diameter.

IV. PROBE CONSTRUCTION

The probe consists of a two-shell construction. The core which holds the ceramic substrate is made entirely of the synthetic microwave material (STYCAST 0005) with a permittivity of 2.54 and a loss tangent of 0.0005. The tip of the outer shell is made of the same material and the main outer shell is made of common PMMA tubing. The core is centered at the tip and held in place with a spring at the connector end. A slight deformation of the outer shell does

Fig. 9. Distribution of the SAR component in the shell phantom parallel to the probe axis measured with a commercial mobile phone.

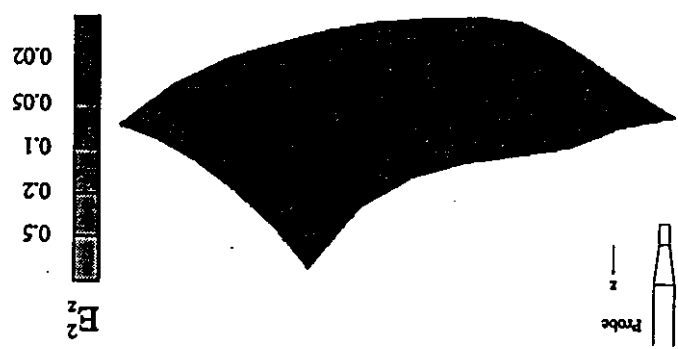
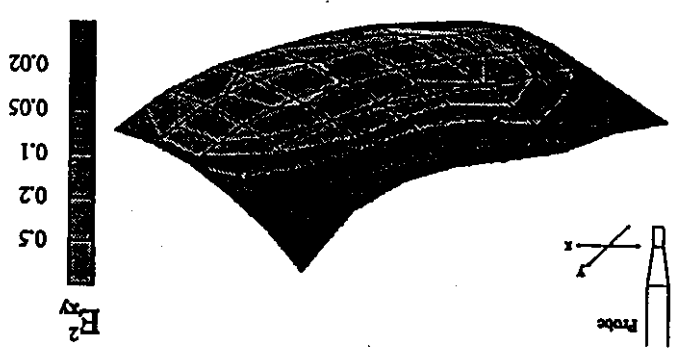


Fig. 8. Distribution of the SAR component normal to the probe axis in the shell phantom measured with a commercial mobile phone.



not effect the fragile core. The probe can be dismantled for repair. Between the core and the outer shell a sheet of high resistivity is introduced to neutralize static charges on the exterior of the probe or in the measuring set up. The distance between the probe tip and the dipole center is 2.7 mm. The probe is connected with a precision 7-terminal connector to the acquisition unit. The counter part in the acquisition unit is flexibly mounted. If excess force is applied to the probe, the probe will give way and a touch detection logic in the acquisition unit will immediately stop the robot. A dielectric tube over the probe connector holds the probe flexibly at a second point 8 cm from the connector. This ensures very high accuracy in the positioning of the probe tip at all probe angles.

V. SURFACE DETECTION

The surface detection system included in the probes consists of an optical multi-fiber line. Half of the fibers are pulsed by an infrared LED, the other half are connected to a synchronized receiver. An object in the correlation area of the two fiber ends causes a coupling between transmitting and receiving fibers. When the probe is moved towards the surface, the reflected signal increases until it reaches a maximum approximately 1.2 mm from the surface, from where it decreases until the probe touches the surface. The location of the maximum is independent of the surface reflectivity and largely independent of the angle between the probe and the surface (see Figure 10). The complete set up gives a positioning accuracy of the probe

- Pulse relays with low thermal voltage ($<0.5 \mu V$) for offset calibration.
- Input filter to prevent HF-signals passing to the amplifier and being rectified in input nonlinearities.
- Electrometer grade differential input amplifier ($<0.1 \mu A$ bias current).
- Second stage instrumentation amplifier with $\times 1 / \times 100$ gain.

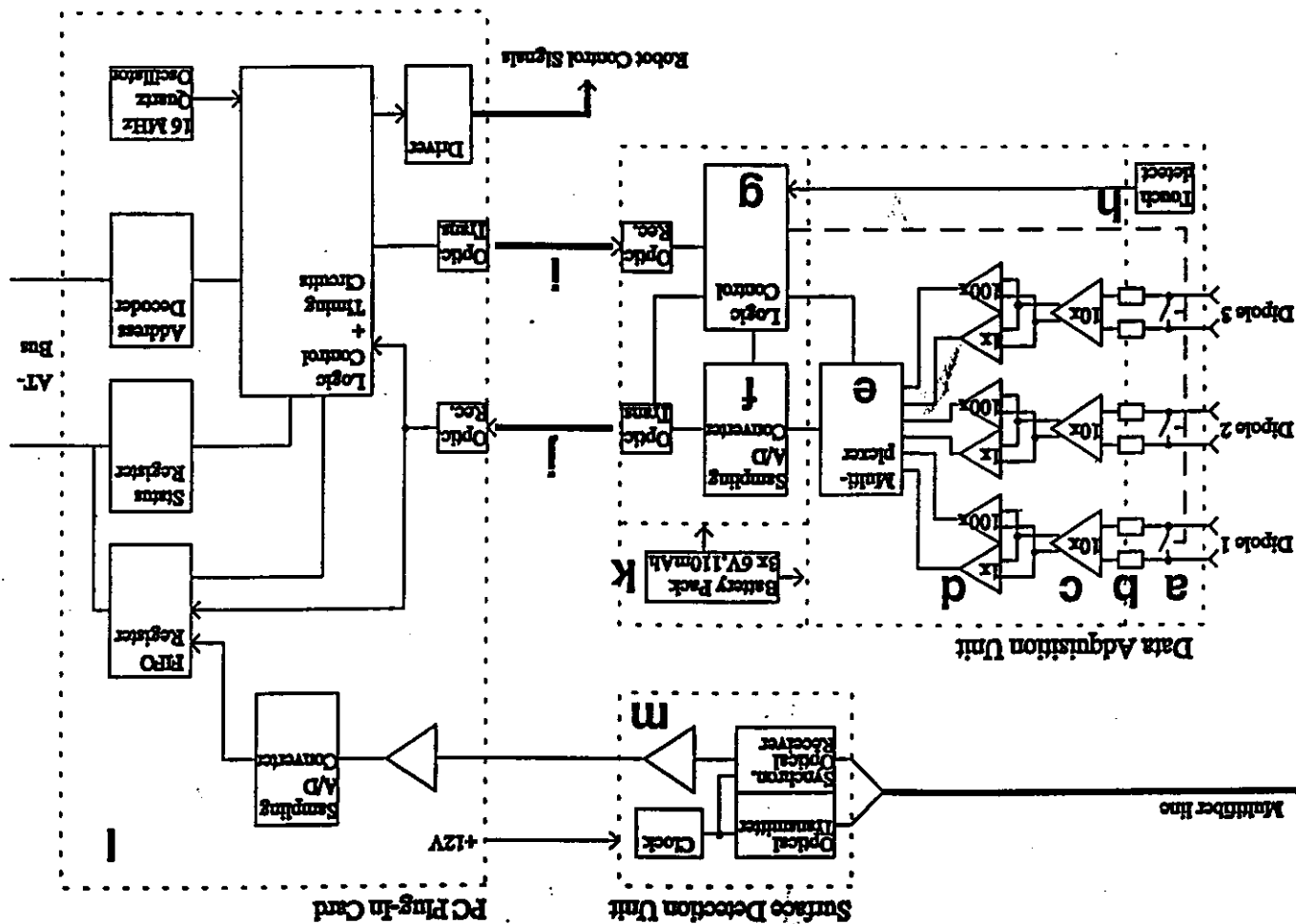
The first unit of the data acquisition system is housed in a metal box of dimensions $68 \times 57 \times 46$ mm, is battery powered and is connected with fiber-optic links to the main data evaluation system. The system can therefore be used in situations where telemetric measurements are necessary. Figure 11 shows the block diagram of the data acquisition system.

The improved probe characteristics were obtained at the cost of increased demands on the signal amplifier. The probes have source impedances of 5 to 8 M Ω due to the high resistive lines and the decoupling filters. The rectified signals range from 1 μV to 200 mV. High noise signals (especially induced signals from power lines) are to be expected.

VI. DATA ACQUISITION ELECTRONICS

with respect to the surface of ± 0.2 mm.

Fig. 11. Block diagram of the data acquisition hardware.



For ease and speed of measurements, a program has been written in C++ under Windows, to perform all involved tasks: Data acquisition, surface detection, robot control, administration of all calibration parameters of the system, evaluation and visualization of the measured data. Complex measuring tasks are available at the push of a button.

VII. SOFTWARE

- Fast 16 bit sampling A/D-converter with serial output.
- Multiplexer to switch between channels and gain.
- Control logic for power down mode, calibration cycle, channel selection, gain selection.
- Touch logic with asynchronous transmission of touch state signal to instantly stop the robot's movement.
- Optical up-link with 1 MHz clock, synchronization and control signals.
- Optical down-link with serial data and state signals (low battery, touch, channel address, etc.).
- Rechargeable battery pack for 5 hours of operation.
- Computer plug in card with main timing unit, data conversion of the serial E-Field data and state signals, data acquisition of the analog signal from the surface detection amplifier and fast digital link to the robot.
- Optical transmitter/receiver for the surface detection system.

of the rectified signal. As long as the signal strength stays follow pulsed HF signals, but provides an average value Because of the low cutoff frequency the system cannot for stronger signals 1 second.

low signal strengths, the measuring time was 10 seconds, for numerical compensation of the diode compression. For the values before and those with the dark symbol show the values for brain tissue. The line with the empty symbol shows the signal strength in V/m and the equivalent SAR values of the signal strength in V/m and the equivalent SAR value. Figure 12 shows the deviation from linearity in function signal-to-noise ratio.

period) varies with the desired accuracy and the received time per grid point (always a multiple of the power line cycle upon reaching the desired accuracy. The measuring accuracy estimate of the filtered signal and stops the measuring cycles accordingly. The program calculates an accuracy switches the gain of the amplifier unit and launches calibration cycles accordingly. Depending on the received signal strength, the program ing data during the measuring or surface detection cycles. for 3D probes. The program reads and filters the incoming data. The data acquisition system samples 7800 data sets per second, i.e., 2600 complete field measurements per second

B. Data Processing

the file and reevaluate the data. false parameters, it is possible to correct the parameters in the calibration parameters. If a measurement is made with an acquisition system is stored in data files together with all played on the screen. The filtered raw data from the data or without surface detection. The measuring process is dis- ments in user defined volumes, planes or along lines with Several measuring options permit complete measure- response times.

modules are downloaded to the robot computer for faster movements can be monitored on the screen. Some program The robot is completely controlled by the PC and its

A. Robot Control

Fig. 10. Response of the surface detector as a function of the distance (x) from the surface.

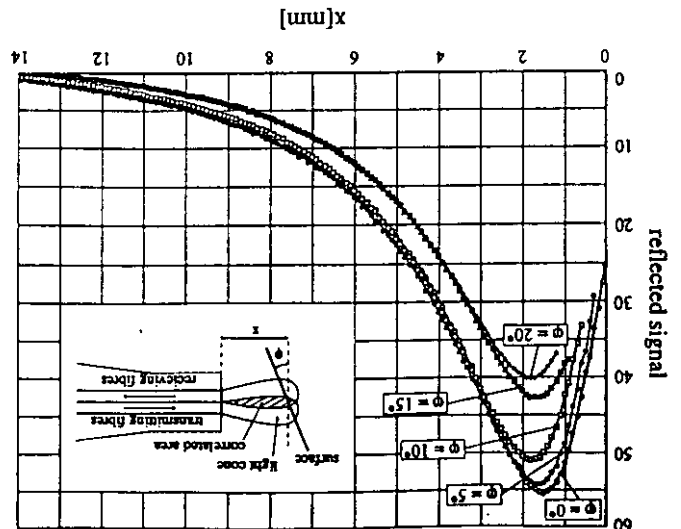


Fig. 13. Measured error between CW and pulsed signals with pulse frequencies between 10Hz and 1kHz and duty cycle between 1 and 100. Reference was a HP437B peak power meter.

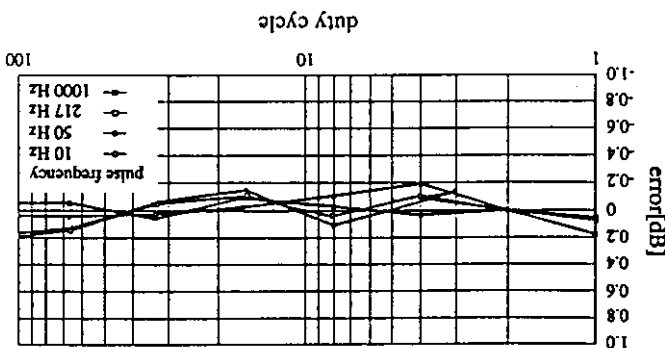
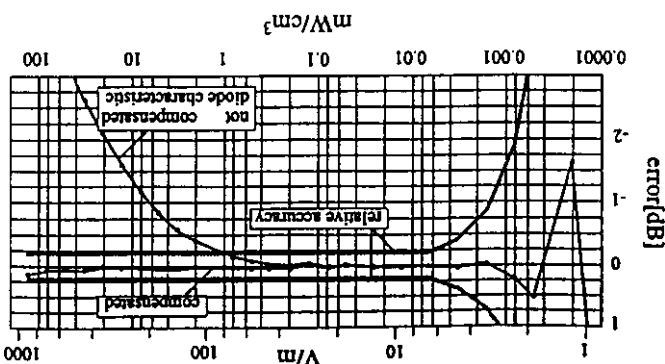


Fig. 12. Deviation from linearity. The line with the dark symbols are the values after compensation of the diode compression. The data was obtained from measurement at 900 MHz in the TEM cell (in 110).



VIII. CALIBRATION AND VALIDATION OF THE SYSTEM

The program evaluates the raw data with the calibration parameters and can produce two-dimensional or three-dimensional graphical output with interpolated isolines in different units (μV of rectified signal, V/m, SAR, power flow density, etc.). The total field strength of each of the dipole components can be separately plotted. SAR values can be numerically integrated over 1 g or 10 g of simulated tissue. Evaluated data can be exported to other file formats. Figures 8 and 9 demonstrate one of the various implemented graphical visualizations.

C. Data Visualization

Figure 13 shows the measured error between CW and pulsed signals with pulse frequencies between 10Hz and 1kHz and duty cycle between 1 and 100. Reference was a HP437B peak power meter.

Figure 13 shows the measured error between CW and pulsed signals with pulse frequencies between 10Hz and 1kHz and duty cycle between 1 and 100. Reference was a HP437B peak power meter.

Fig. 13. Measured error between CW and pulsed signals with pulse frequencies between 10Hz and 1kHz and duty cycle between 1 and 100. Reference was a HP437B peak power meter.

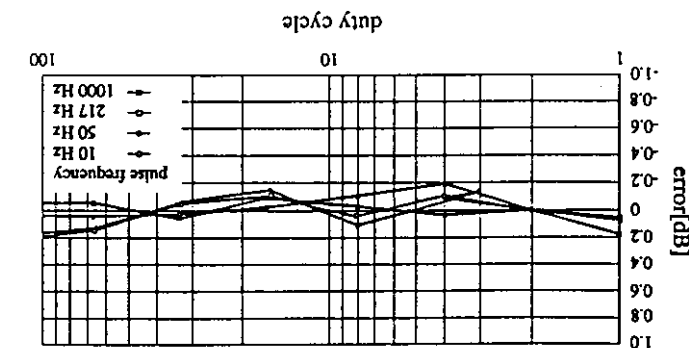


Fig. 12. Deviation from linearity. The line with the dark symbols are the values after compensation of the diode compression. The data was obtained from measurement at 900 MHz in the TEM cell (in 110).

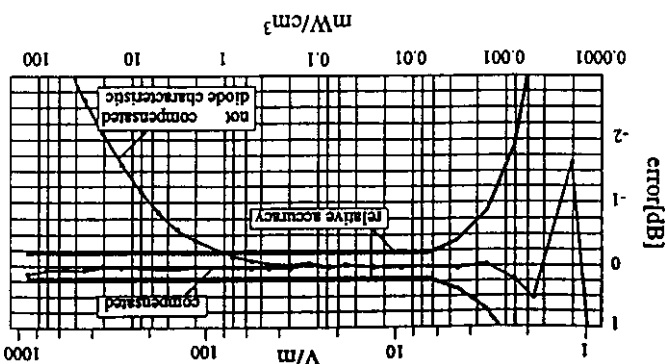


TABLE I

SYSTEM SPECIFICATIONS WITH ISOTROPIC E-FIELD.

frequency range	10 MHz to > 3 GHz
dynamic range in tissue simulating solutions	1 μ W/g to 100 mW/g
linearity	> ± 0.2 dB
deviation from isotropy in tissue (triangular probe)	± 0.2 dB
- normal to probe axis	± 0.8 dB
- in all planes, all polarizations	> ± 0.2 dB
variation with frequency	> ± 0.2 dB
spatial resolution of SAR measurements	> 0.125 cm ³
reproducibility of probe positioning	> ± 0.2 mm

Note: The rather large deviation from isotropy in all planes scarcely affects the accuracy of dosimetric assessments if the probe is positioned predominantly normal to the phantom surface.

less than 0.5 mm allowing true point measurements. However, high power is required because of the rather low sensitivity (> 10 mW/g). Figure 14 shows the results of the three evaluation methods at different distances from the transmitting dipole and the probe from the bottom of the phantom.

IX. CONCLUSION

The developed measurement system is a flexible, automated, time-efficient tool to assess SAR distributions in tissue simulating solutions. It is especially suited for compliance testing of handheld or body mounted devices with specific safety standards. Tests have shown an excellent reproducibility of the integrated peak SAR values of well within $\pm 5\%$ even when changing the starting measuring grid. The specifications of the system can be summarized as in Table I.

Although the main emphasis is now on the open phantom issue, several improvements are anticipated. For instance, extension of the system for general near field measurements used in antenna design, EMI, EMC.

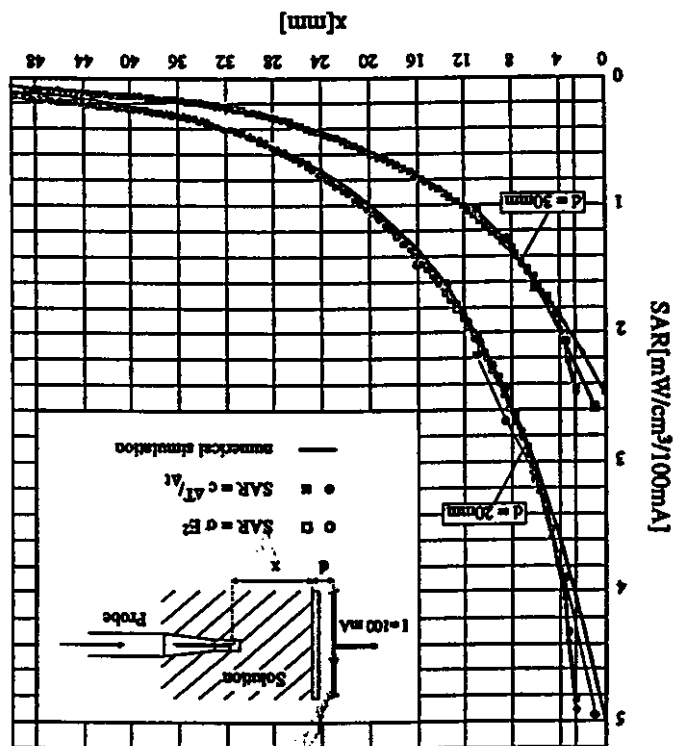
ACKNOWLEDGEMENTS

The development of this scanning system was supported by the Federal Ministry of Posts and Telecommunications (Germany), Deutsche Telekom (Germany), Swiss Telecom PTT (Switzerland) and Mannesmann GmbH (Germany). The authors gratefully acknowledge the help of Mr. Klaus Meier, Mr. Martin Schmid, Mr. Jeron de Keijzer, as well as valuable advice of Dr. Quintino Balzano and Mr. Oscar Garay.

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Fig. 14. Comparison of SAR values obtained by numerical simulation, measured temperature rise and E-field measurements for a plane phantom exposed to a half wave 900 MHz dipole parallel to the phantom's surface. The phantom was filled with brain equivalent solution ($\epsilon_r = 44$, $\sigma = 1.1$ mho/m). All values are normalized to an antenna feedpoint current of 100 mA.



In solutions, however, a conversion factor must be introduced to account for the different sensitivities of the probes in the solution. This conversion factor was obtained by comparing the measured values with those from numerical simulations. The simple set up was already used in [2] and consists of a standard half wave dipole below a half plane phantom.

To validate the result, the same set up was used with a 100 W amplifier and temperature measuring equipment. The fiber optical temperature probes have a diameter of

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Appendix 2

pages 1 - 9

PROBE ET3DV4 SN: 1105

Probe ET3DV4

SN:1105

Manufactured:	May 1995
Calibrated:	July 1997
Recalibrated:	August 1998

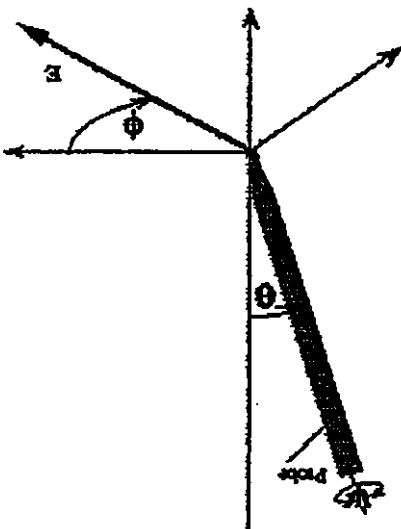
Calibrated for System DASY2

Introduction

The performance of all probes is measured before delivery. This includes an assessment of the characteristic parameters, receiving patterns as a function of frequency, frequency response and relative accuracy. Furthermore, each probe is tested in use according to a dosimetric assessment protocol. The sensitivity parameters (NormX, NormY, NormZ), the diode compression parameter (DCP) and the conversion factor (ConvF) of the probe and some of the measurement diagrams are given in the following.

The performance of the individual probes varies slightly due to tolerances arising from the manufacturing process. Since the lines are highly resistive (several MOhms), the offset and noise problem is greatly increased if signals in the low μV range are measured. Accurate measurement below 10 $\mu V/g$ are possible if the following precautions are taken. 1) check the current grounding with the *multimeter*, i.e., low noise levels, 2) compensate the current offset, 3) use long integration time (approx. 10 seconds), 4) *calibrate* before each measurement, 5) persons should avoid moving around the lab while measuring.

Fig. 1: Due to the field distortion caused by the supporting material, the probe has two characteristic directions, referred to as angle ψ and θ .



The probes are calibrated in the TBM cell in 110 although the field distribution in the cell is not very uniform and the frequency response is not very flat. To ensure consistency, a strict protocol is followed. The conversion factor (ConvF) between this calibration and the measurement in the tissue simulation solution is performed by comparison with temperature measurements and computer simulations. If measurements have to be performed in solutions with other electrical properties or at other frequencies, the conversion factor has to be assessed by the same procedure. As the probes have been constructed with printed resistive lines on ceramic substrates (thick film technique), the probe is very delicate with respect to mechanical shocks.

Attention:

Do not drop the probe or let the probe collide with any solid object. Never let the robot move without first activating the emergency stop feature (i.e., without first turning the data acquisition electronics on).

DASY2 - Parameters of Probe: ET3DV4 SN:1105

Sensitivity in Free Space

NormX	1.51	$\mu\text{V}/(\text{V}/\text{m})^2$
NormY	1.57	$\mu\text{V}/(\text{V}/\text{m})^2$
NormZ	1.41	$\mu\text{V}/(\text{V}/\text{m})^2$

Diode Compression

DCP X	41000	μV
DCP Y	41000	μV
DCP Z	41000	μV

Sensitivity in Tissue Simulating Liquid

450 MHz	ConvF X	6.6	extrapolated			
450 MHz	ConvF Y	6.6	extrapolated			
450 MHz	ConvF Z	6.6	extrapolated			
800 MHz	ConvF X	6.0	$\pm 10\%$			
800 MHz	ConvF Y	6.0	$\pm 10\%$			
800 MHz	ConvF Z	6.0	$\pm 10\%$			
1500 MHz	ConvF X	5.3	interpolated			
1500 MHz	ConvF Y	5.3	interpolated			
1500 MHz	ConvF Z	5.3	interpolated			
1800 MHz	ConvF X	4.9	$\pm 10\%$			
1800 MHz	ConvF Y	4.9	$\pm 10\%$			
1800 MHz	ConvF Z	4.9	$\pm 10\%$			

$\epsilon_r =$	48 $\pm$ 5%					
$\sigma =$	0.50 $\pm$ 10% mho/m					
	(brain tissue simulating liquid)					

$\epsilon_r =$	42.5 $\pm$ 5%					
$\sigma =$	0.86 $\pm$ 10% mho/m					
	(brain tissue simulating liquid)					

$\epsilon_r =$	41 $\pm$ 5%					
$\sigma =$	1.32 $\pm$ 10% mho/m					
	(brain tissue simulating liquid)					

$\epsilon_r =$	40.5 $\pm$ 5%					
$\sigma =$	1.659 $\pm$ 10% mho/m					
	(brain tissue simulating liquid)					

Sensor Offset

Probe Tip to Sensor Center
Surface to Probe Tip

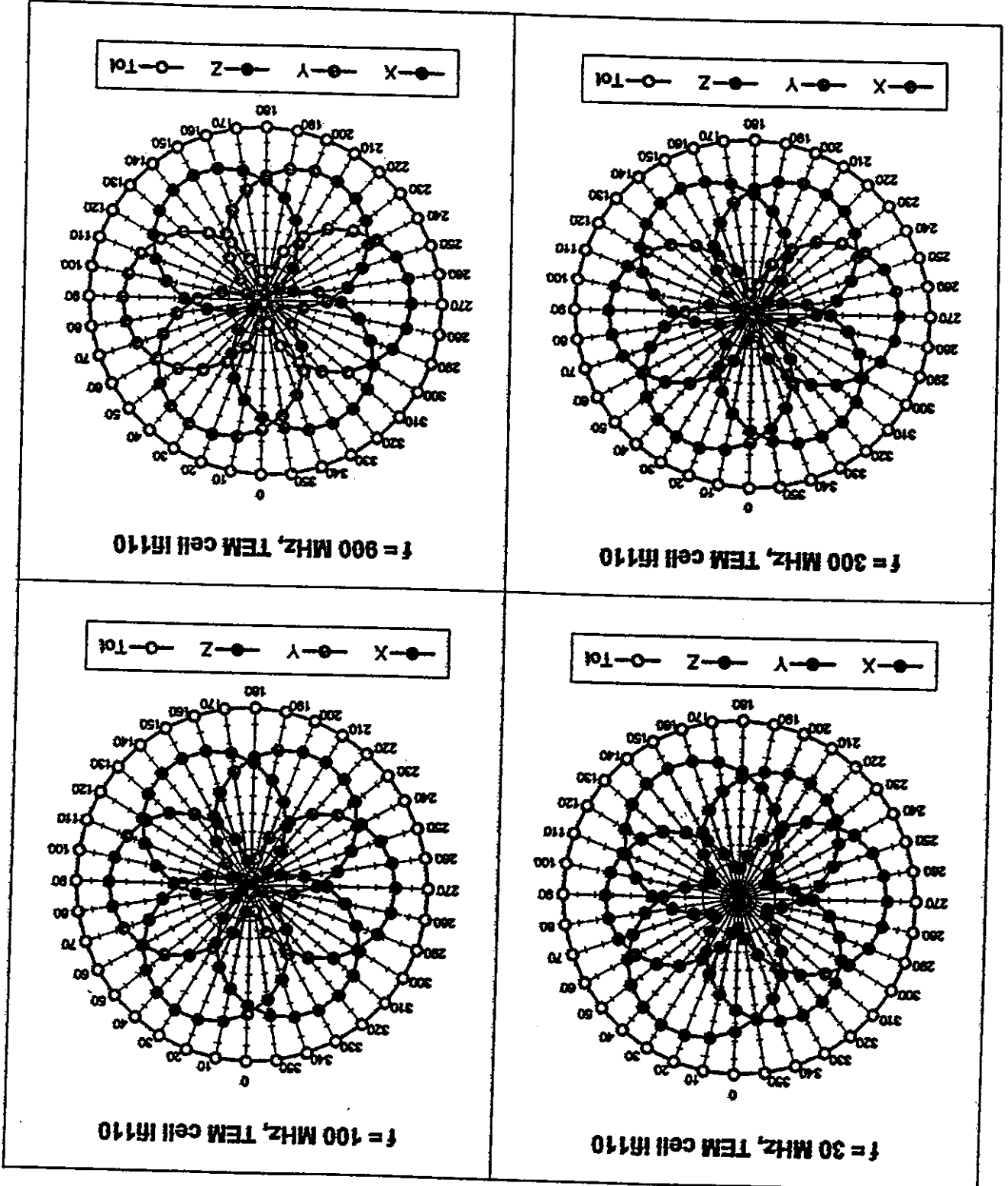
2.7

1.4 $\pm$ 0.2

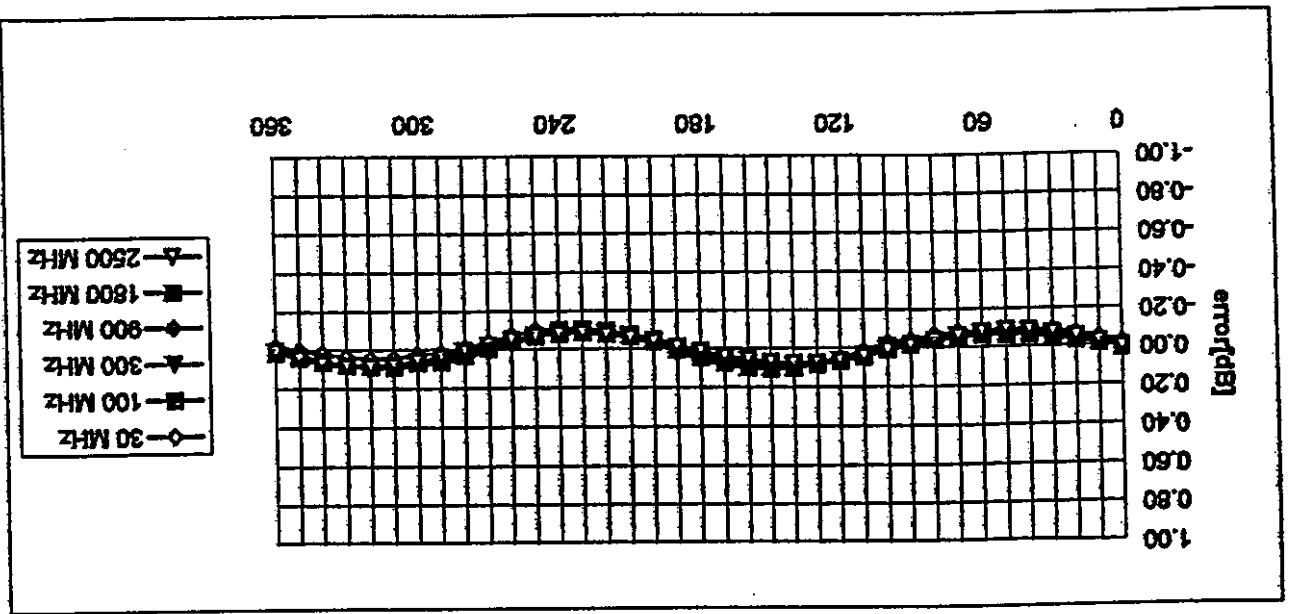
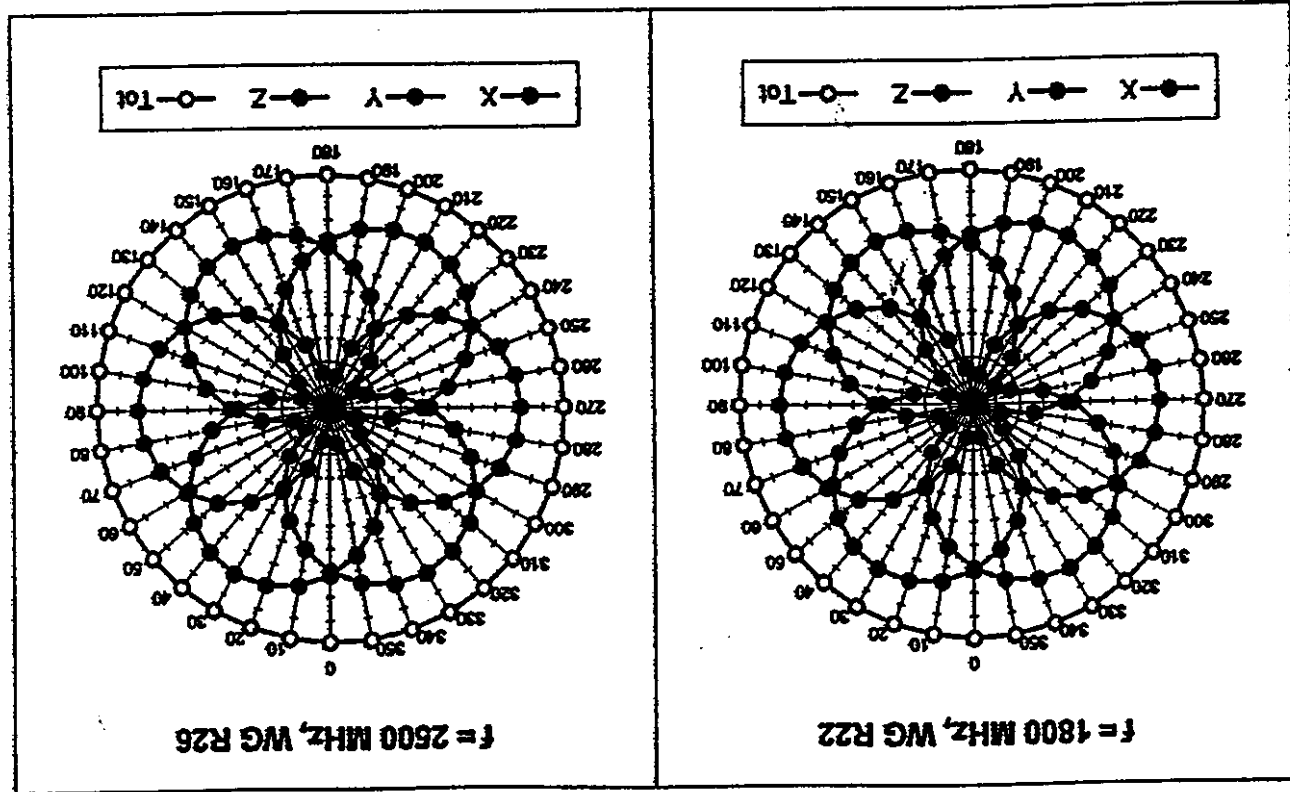
mm

mm

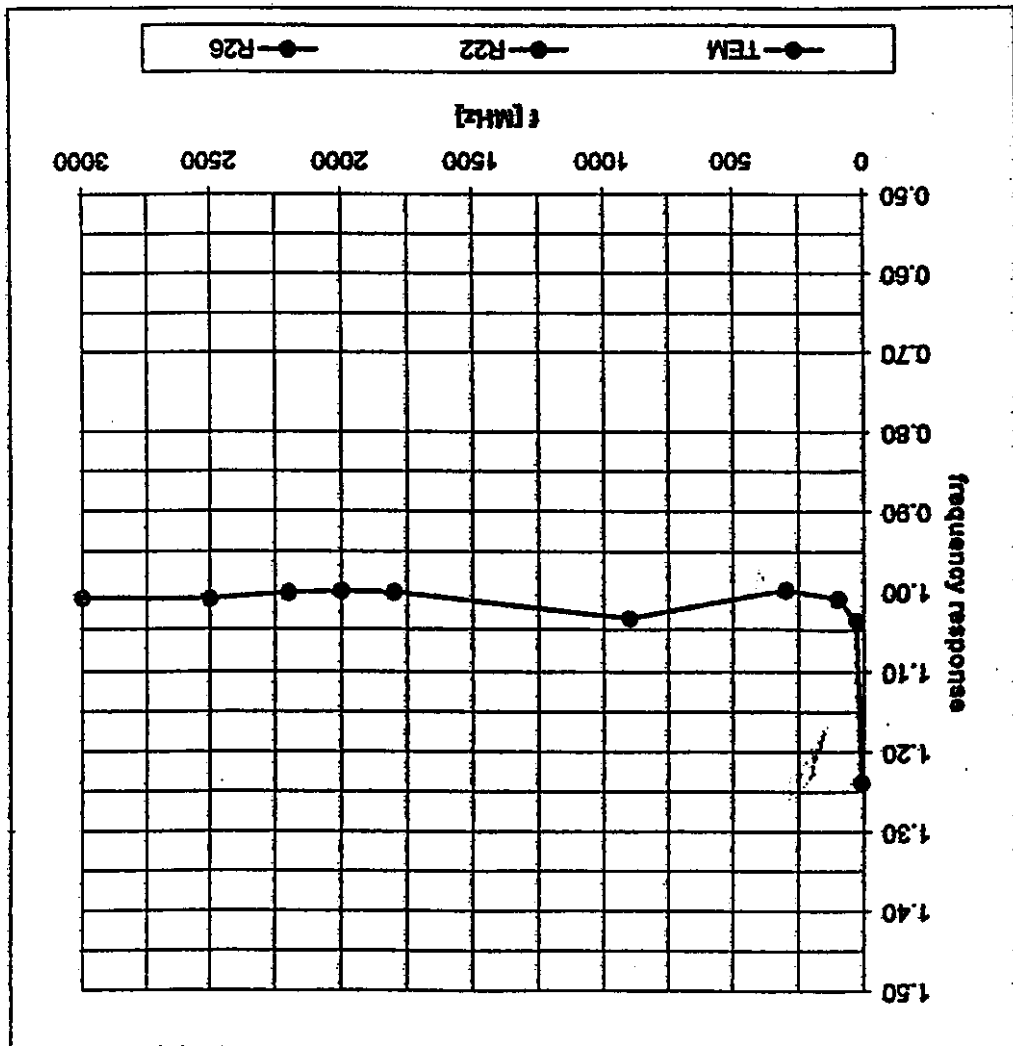
Receiving Pattern (ϕ), $\theta = 0^\circ$



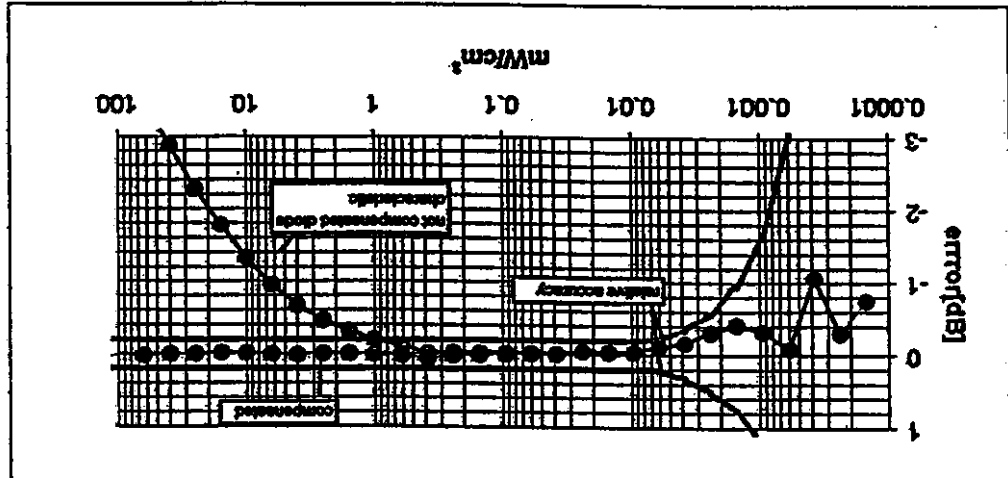
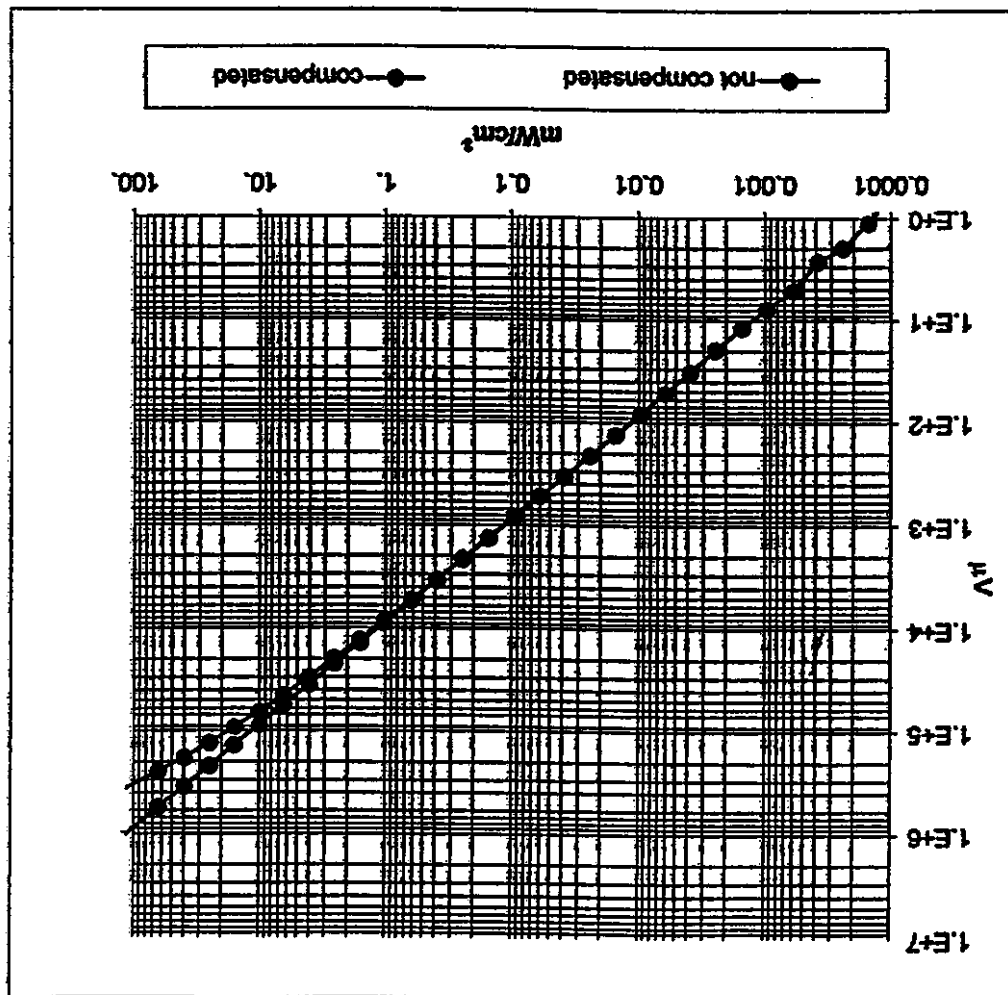
Isotropy Error (ϕ), $\theta = 0^\circ$



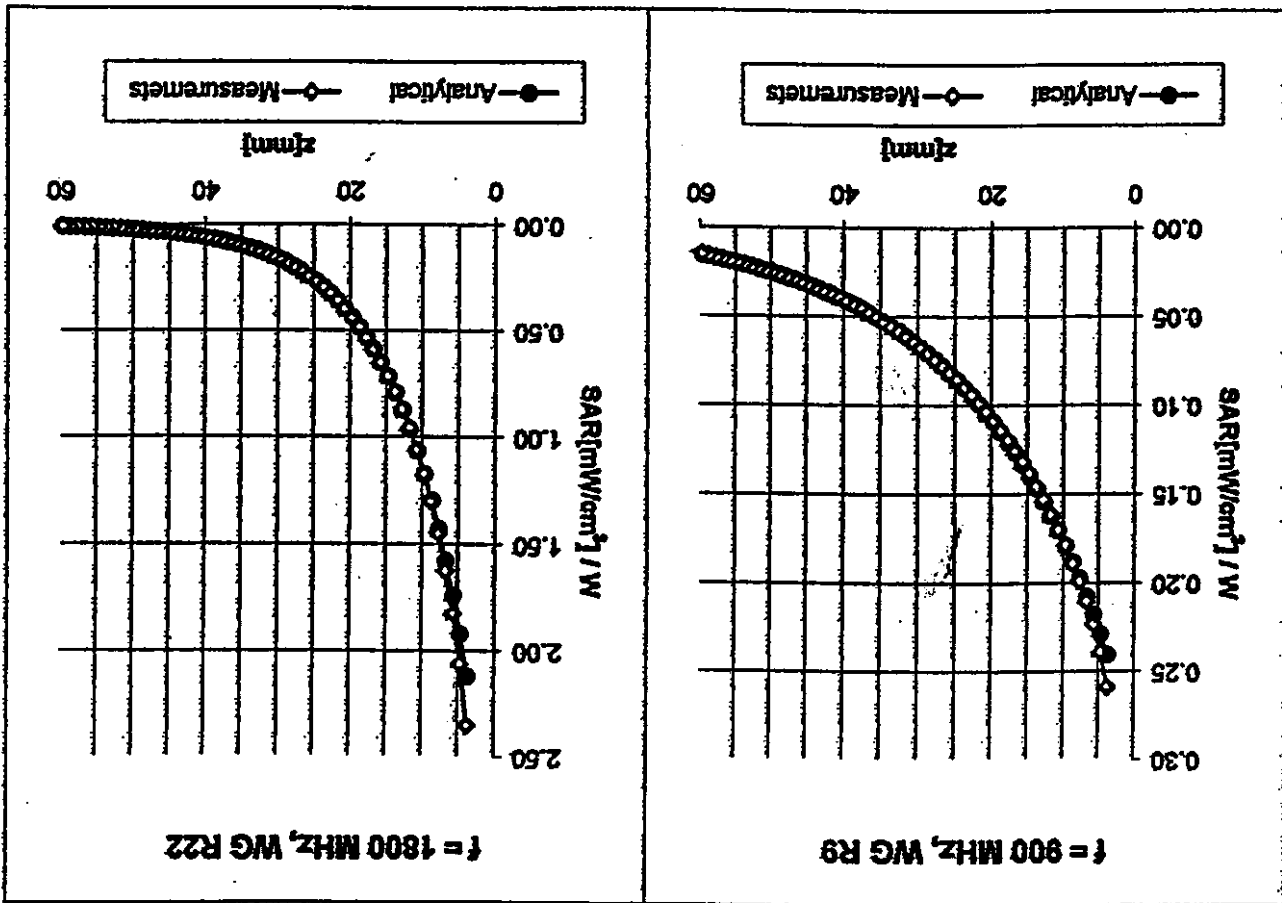
Frequency Response of E-Field (TEM-Cell:11110, Waveguide R22, R26)



Dynamic Range f(SAR_{brain}) (TEM-Cell:11110)

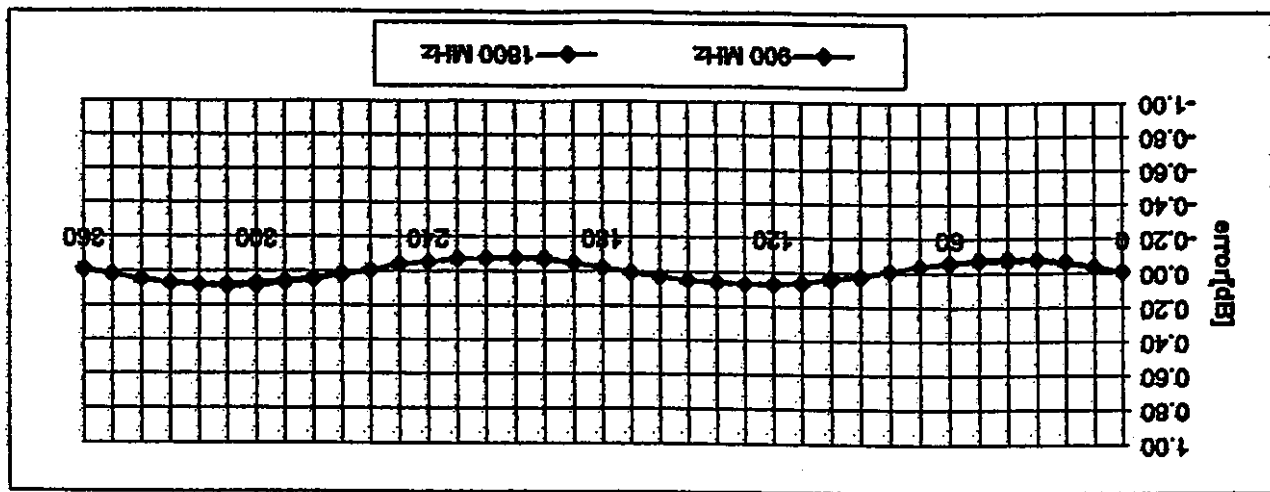


Conversion Factor Assessment



Receiving Pattern (ϕ)

(in brain tissue, z = 5 mm)



Appendix 3

pages 1 - 5

DASY- DOSIMETRIC ASSESSMENT SYSTEM
CALIBRATION REPORT
DATA ACQUISITION ELECTRONICS

DASY - DOSIMETRIC ASSESSMENT SYSTEM

CALIBRATION REPORT

DATA ACQUISITION ELECTRONICS

MODEL:

DASY 2

SERIAL NUMBER:

218

This Data Acquisition Unit was calibrated and tested using a FLUKE 702 Process Calibrator. Calibration and verification were performed at an ambient temperature of $23 \pm 5^\circ\text{C}$ and a relative humidity of $< 70\%$.

Measurements were performed using the standard DASY software for converting binary values, offset compensation and noise filtering. Software settings are indicated in the reports.

Results from this calibration relate only to the unit calibrated.

Calibrated by:

M. Bruggmann

Calibration Date:

6.8.1998

DASY Software Version:

DASY3 V1.0B

1. DC Voltage Measurement

DA - Converter Values from DAE

High Range: 1LSB = 6.1 μ V, full range = 400 mV
 Low Range: 1LSB = 61nV, full range = 4 mV

Software Set-up: Calibration time: 3 sec Measuring time: 3 sec

Setup	X	Y	Z
High Range	400	400	400
Low Range	4	4	4
Connector Position	0°		

High Range	Input	Reading in μ V	% Error
Channel X + Input	200mV	200484.8	0.24
	20mV	20052.84	0.26
Channel X - Input	20mV	-20044.08	0.22
Channel Y + Input	200mV	200692.8	0.35
	20mV	20070.9	0.35
Channel Y - Input	20mV	-20062.35	0.31
Channel Z + Input	200mV	200779.3	0.39
	20mV	20080.92	0.40
Channel Z - Input	20mV	-20071.6	0.36

Low Range	Input	Reading in μ V	% Error
Channel X + Input	2mV	2004.037	0.20
	0.2mV	200.4825	0.24
Channel X - Input	0.2mV	-201.2267	0.61
Channel Y + Input	2mV	2010.955	0.55
	0.2mV	201.1715	0.59
Channel Y - Input	0.2mV	-201.258	0.63
Channel Z + Input	2mV	2011.045	0.55
	0.2mV	201.405	0.70
Channel Z - Input	0.2mV	-201.272	0.64

2. Common mode sensitivity

Software Set-up
Calibration time: 3 sec, Measuring time: 3 sec
Low Range

in μV	Common mode Input Voltage	High Range Reading	Low Range Reading
Channel X	200mV	-15.01851	-16.37388
	- 200mV	3.9423	5.190906
Channel Y	200mV	-5.942738	-12.73525
	- 200mV	8.959845	14.79019
Channel Z	200mV	-13.70552	-7.222769
	- 200mV	13.74889	1.222047

3. Channel separation

Software Set-up
Calibration time: 3 sec, Measuring time: 3 sec
High Range

in μV	Input Voltage	Channel X	Channel Y	Channel Z
Channel X	200mV	-	-2.15438	-3.630622
Channel Y	200mV	-3.786761	-	-2.68589
Channel Z	200mV	-11.63471	-3.185863	-

4. AD-Converter Values with inputs shorted

in LSB	Low Range	High Range
Channel X	15341.1	16472.43
Channel Y	17057.39	16493.9
Channel Z	15677.94	16476.23

5. Input Offset Measurement

Measured after 15 min warm-up time of the Data Acquisition Electronic.
Every Measurement is preceded by a calibration cycle.

Software set-up:

Calibration time:

3 sec

Measuring time:

3 sec

Number of measurements: 100, Low Range

Input 10M Ω				
In μ V	Average	min. Offset	max. Offset	Std. Deviation
Channel X	-0.54654	-1.7898	0.5676	0.6451
Channel Y	-0.46657	-1.2647	0.56467	0.52184
Channel Z	-0.04984	-1.9876	1.0168	0.65748

Input shorted				
In μ V	Average	min. Offset	max. Offset	Std. Deviation
Channel X	-0.1067	-0.65465	0.46841	0.6577
Channel Y	-0.41078	-0.7414	0.4235	0.46574
Channel Z	0.4218914	-0.46771	0.5719	0.79841

6. Input Offset Current

In fA	Input Offset Current
Channel X	< 100
Channel Y	< 100
Channel Z	< 100

7. Input Resistance

	Calibrating	Measuring
Channel X	199.6 k Ω	20.2 M Ω
Channel Y	199.7 k Ω	20.2 M Ω
Channel Z	199.2 k Ω	20.2 M Ω

8. Low Battery Alarm Voltage

In V	Alarm Level
Supply (+ Vcc)	5.3 V
Supply (- Vcc)	-5.6V

9. Power Consumption

In mA	Switched off	Stand by	Transmitting
Digital Supply (VCC)	0.011	4.72	12.2
Analog Supply (+ Vcc)	0.003	9.89	9.94
Analog Supply (- Vcc)	0.1	-9.7	-9.8

10. Functional test

Touch async pulse 1	ok
Touch async pulse 2	na
Touch status bit 1	ok
Touch status bit 2	na
Remote power off	ok
Remote analog Power control	ok

Date: 6.8.98

Signature: M. Buzgum

INDUSTRIAL ROBOT AND CONTROL UNIT

Appendix 4

page 1

INDUSTRIAL ROBOT AND CONTROL UNIT

General		Work envelope		Load capacity		Performance		Control unit		Work environment		Weight
Axes	6	Reaches at tool flange	985 mm	Normal payload	6 kg	Repeatability	± 0.02 mm (constant temperature)	CPU	Motorola 68030	Temperature	5 to 40° C (CEI 204-1)	105 kg
Drives	AC Brushless electric motors	Reach at wrist center	900 mm	Maximum payload	9 kg (at low speed)	Maximum speed	9.8 m/s	FPU	Motorola 68882	Humidity	< 90 % non condensing (CEI 204-1)	200 kg
Control	Digital	Working volume	360° working volume in left or right	Tool Flange	ISO 9409 - 1 - A 40	Cartesian speed	1.5 m/s	Options	12 In/8 Out in standard version, expandable to 64 In/64 Out by 32 In/32 Out module	Interference suppression	50/60 Hz - 4 KVA	
Positional Control	Absolute resolvers, non-volatile	Working range	Axes 1 - Axes 2 - Axes 3 - Axes 4 - Axes 5 - Axes 6	Normal payload	9 kg (at low speed)	Cartesian speed	1.5 m/s	IO Interface	1 RS-422/485 serial ports	Power supply	230, 400, 440, 480 V 3-phase incorporated	
Coordinates	Cartesian, revolute	configuration	Axes 1 - Axes 2 - Axes 3 - Axes 4 - Axes 5 - Axes 6	Maximum payload	9 kg (at low speed)	Maximum speed	9.8 m/s	Programming	3 RS-232 serial ports			
Structure	Revolute								1 RS-422/485 serial ports			
Interconnecting cables	5 m (between arm and control unit)								Analogue inputs/outputs			
									10 m interconnecting cables (between arm and control unit)			
									RAM : 4 Mbytes, expandable to 8 Mbytes			
									Hard disk : 40 Mbytes minimum			
									Built in 3 1/2" disk drive			
									(1.44 Mbytes) IBM PC format			

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Appendix 5

pages 1 - 3

BRAIN TISSUE SIMULATING LIQUID

Brain Tissue Simulating Liquids

Preparation of the Liquids

Requirements:

- Scale
- Magneto Stirrer: Heating Plate, Magnetos (recommended).
- HP 85070A Dielectric Probe Kit (200MHz to 20GHz) plus mounting device and Network Analyser
- Canisters or "closed" jars to store the liquid (recommended)

Preparation:

- 1.) Heat the water to about 40° Celsius.
- 2.) Add salt and bactericide to water while stirring and wait until salt is dissolved.
- 3.) Add about one third of the sugar. Keep stirring. Wait until sugar is dissolved. Add the second third and when dissolved add the final third. The liquid gains volume and thickens slightly.
- 4.) Keep stirring at maximum speed possible.
- 5.) When all the sugar is dissolved, add the HEC. HEC is highly hygroscopic. It forms lumps when added to the liquid. Either "help" the magneto stirrer by stirring from outside or dissolve all of the HEC first in another jar with a little bit of liquid using another stirrer. Add it then to the rest of the solution. Once HEC is added the liquid thickens considerably.
- 6.) During the whole process watch the temperature to prevent water evaporation.
- 7.) Once the liquid clears up pour it into canisters. Let it stand for a couple of hours before using it.

III Use

- When in the item (phantom models), monitor water evaporation.
- To minimize water evaporation cover the phantoms when not used. Do not store the liquid in the phantoms, rather store it in closed canisters.
- In case water has evaporated, you can add (warm) water to the liquid. Be sure that after stirring it is completely homogeneous.
- The liquid can be used for at least 3 months. After longer periods bacteria might grow that are resistant against the bactericide.

Recipe 900 MHz:

Water 40.1 %
Sugar 58.0 %
Salt (NaCl) 0.8 %
HBC (Hydroxyethylcellulosis) 1.0 %
Preservative Substance

900 MHz: $\epsilon_r = 42.5 \pm 5\%$ and $\sigma = 0.85 \pm 10\%$ mho/m

Recipe 1800 MHz:

Water 45.0 %
Sugar 53.9 %
HBC (Hydroxyethylcellulosis) 1.0 %
Preservative Substance

1800 MHz: $\epsilon_r = 41.0 \pm 5\%$ and $\sigma = 1.65 \pm 10\%$ mho/m

Parameters of Probe ET3DV4 SN:1105

NormX	1.53	$\mu V/(V/m)^2$
NormY	1.6	$\mu V/(V/m)^2$
NormZ	1.42	$\mu V/(V/m)^2$
DCP	43000	μV
ConvF(450MHz)	6.64 ± 10%	$\epsilon_r=47.2 \pm 5\%; \sigma=0.45 \pm 10\% \text{ mho/m}^1$
ConvF(900MHz)	5.98 ± 10%	$\epsilon_r=42.5 \pm 5\%; \sigma=0.86 \pm 10\% \text{ mho/m}^1$
ConvF(1800MHz)	4.85 ± 10%	$\epsilon_r=41.0 \pm 5\%; \sigma=1.7 \pm 10\% \text{ mho/m}^1$
$d_{\text{probe_tip - center_dipoles}}$	2.7	mm
$d_{\text{surface - probe_tip}}$	1.2 ± 0.2	mm

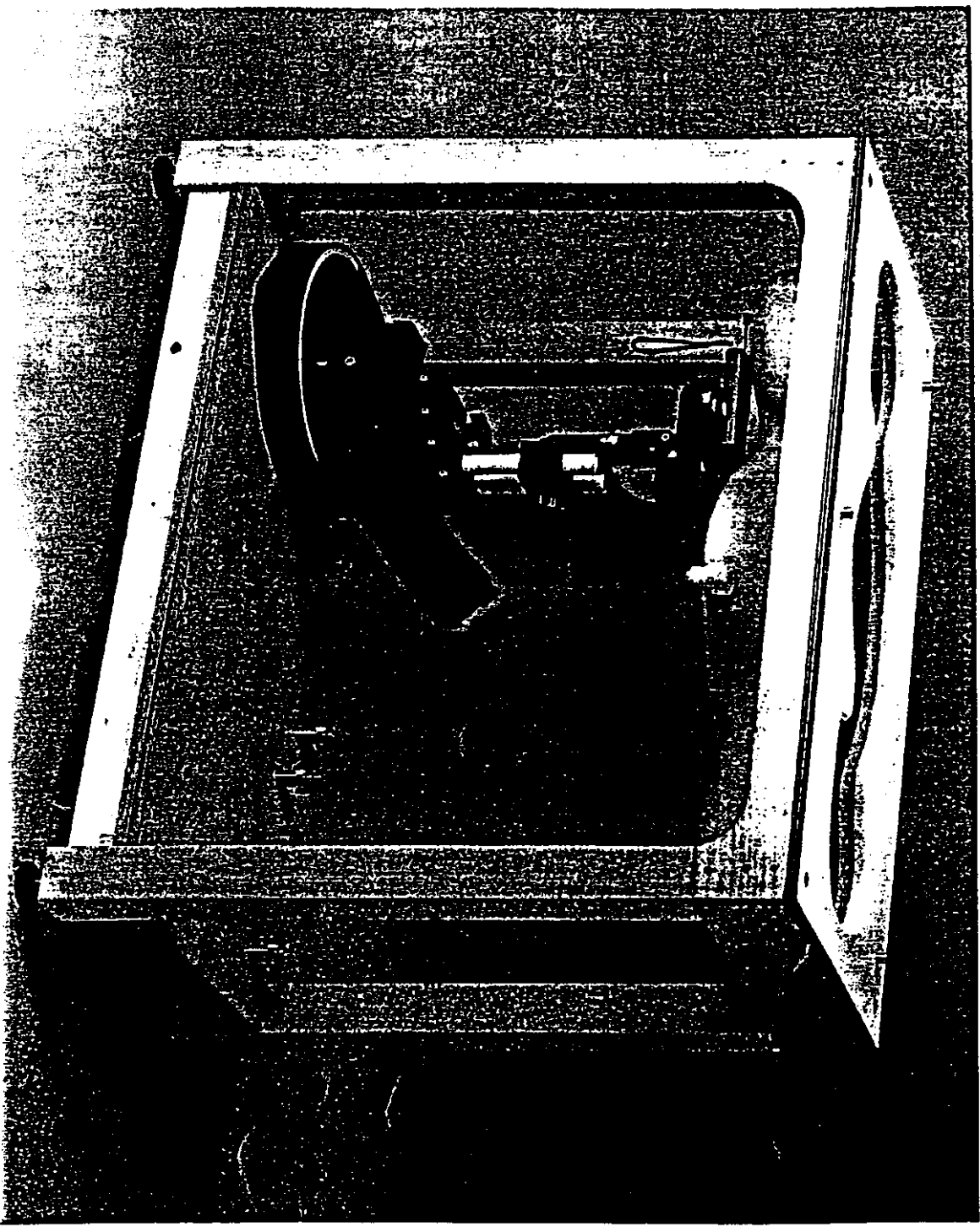
¹ Brain tissue simulating liquids

Appendix 6

pages 1 - 2

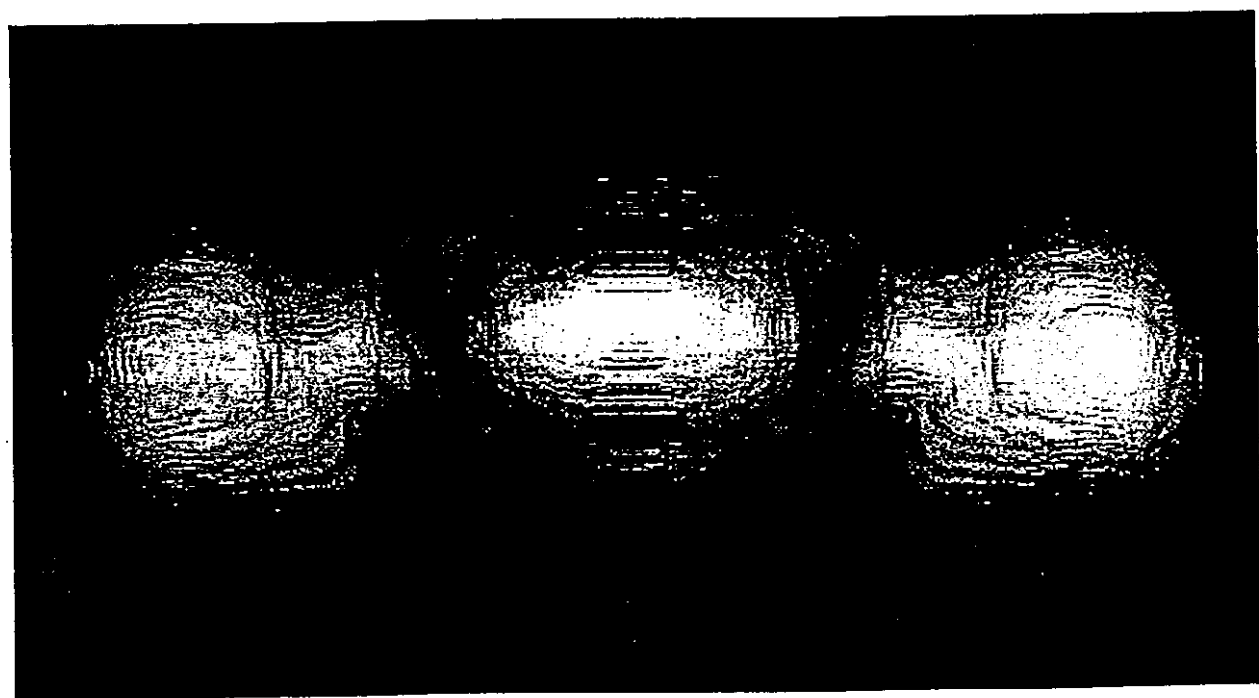
GENERIC TWIN PHANTOM
Version 3.

Version 3



ADVANCED INFORMATION 7/96

OPTIMIZED PHANTOM WITH IMPROVED MOUNTING DEVICE FOR MTE



Summary

In cooperation with ETH Zurich, Schmid & Partner Engineering AG is currently developing a new phantom, as well as a new device for the mounting and positioning of handheld mobile telecommunications equipment (MTE). This new phantom setup will be optimized for compliance testing in accordance with CENELEC, ANSI/IEEE and NCRP requirements. It will have the following improvements compared to the current setup (Left/Right-Hand Torso V2.1 and Mounting Device for Transmitters V2.0):

- Basis**
The new phantom will be based on an anatomical study.
- Shape**
The shape of the new phantom will be designed to provide SAR values which are unlikely to be exceeded in the head of any user. Furthermore, the overestimation will be minimal.
- Modeling of the Ear**
The phantom will include a simple ear segment which represents the thickness of the pressed human ear.
- Construction**
The new phantom will also be made of fibreglass. However, the tolerance of the shell thickness will be substantially improved. The fibreglass shell will be integrated into a wooden table which will further improve the stability of the phantom.
- Mounting Device**
The mounting device for the MTE will allow accurate and repeatable placement of the device with respect to the positions defined in the latest CENELEC draft. The repeatability of the horizontal position shall be better than ± 1 mm. It will be designed to be compatible with current MTE designs and anticipated future designs.
- User-Friendliness**
The phantom will also be more user-friendly, since left and right hand configurations and the device for mounting and positioning of the MTE will be combined in one setup, i.e., left and right hand measurements will be possible without exchanging phantoms. The minimum amount of stimulation liquid to test MTE with operating frequencies above 800 MHz will be reduced.
- Compatibility**
The phantom will be fully compatible with the hardware and software of DASY2 as well as of DASY3. (DASY3 will be available in late Spring 97.)
- Availability**
The new phantom and the new device for the mounting and positioning of MTE will be commercially available in October 1996. The shape of the phantom will be available as a CAD data set on the Internet.

Appendix 7

pages 1 - 11

PROBE CALIBRATION

Institut für Feldtheorie
und Hochfrequenztechnik
ETH Zürich
CH-8092 Zurich

Mr. Mikka Pankinaho
Nokia Mobile Phones
NMP/R&D
P.O. Box 86
FIN-24101 Salo
Finland

Zurich, 2 December 1995

Mobile Phone Certification

Dear Mr. Pankinaho, / L K K A

In mid-September, we promised to send preprints of the paper which describes the calibration procedure we developed during the last months. We would appreciate any suggestions and comments, since a thorough calibration is fundamental to enforce the safety limits. In addition, we would like to take this opportunity to inform you about the newest developments towards finalizing the scientific and technical conditions for a type approval.

Uncertainties of Measurements: In connection with the calibration, we performed an analysis which assessed the total uncertainty of SAR measurements in shell phantoms. The results are promising. The total uncertainty can be kept below $\pm 20\%$ at 900 MHz. A project to further reduce these uncertainties and to develop a standard calibration procedure has now been submitted to the EU program "Standards, Measurements & Testing."

Phantom: Another open issue is the verification that the absorption in homogeneous human phantoms represents well the actual spatial peak absorption in the user. In one study, in close cooperation with the research center of German Telekom, absorption induced in three numerical and three experimental phantoms were compared for the mobile communications frequency at 900 MHz. The various phantoms and our findings are briefly described in the attachment.

Requirements of a Certification Procedure: In connection with the recent WTR workshop in Rome, we defined the scientific pre-condition necessary to implement a certification procedure. The manuscript also reflects the requirements which were discussed within CENELEC's TC111 Working Group on Mobile Telecommunications Equipment. Please find the manuscript in the attachment as well.

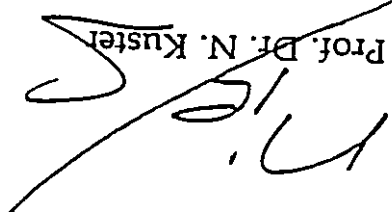
DASY: Schmid & Partner Engineering AG (SPEAG) has started the development of DASY3. Besides a general revision and extension of the DASY2 hardware and software, the main objectives of DASY3 are improved spatial resolution, improved precision and improved time efficiency. DASY3 will be largely compatible with DASY2, although some of the new functions will not be fully usable without minor hardware updates. SPEAG will keep you informed with respect to these developments.

The temperature probes which have been developed for the previously mentioned calibration study will soon be commercially available. The prototype showed a sensitivity of about <0.1 mK/s. It might be interesting to all DASY users that this probe will be fully compatible with DASY2, DASY3 and DASYmini. The active volume of about 1 mm^3 is ideal for those laboratories which plan to do calibration or SAR measurements in very small structures.

Part of the industry was interested in a video of DASY2 to demonstrate the test procedure to their customers. Since we already had a video for other occasions, we adapted it to these requests and now have copies available. If you are interested, please return the enclosed form by mail or fax. If you want copies of any of the publications listed on that form, we would be happy to send you these copies as well.

If you have any questions regarding our activities in the area of mobile phone certification, please do not hesitate to contact me. For questions regarding the dosimetric assessment system DASY, I suggest you contact SPEAG directly (phone: +41 52 232 7272, FAX: +41 52 232 7127).

Yours sincerely


Prof. Dr. N. Kuster
Encl.

Broadband Calibration of E-Field Probes in Lossy Media

Klaus Meier, Michael Burkhardt, Thomas Schmid and Niels Kuster

published so far about broadband calibration of isotropic E-field probes in dielectric materials. In [3] a calibration procedure in an S-band waveguide at a single frequency of 2.45 GHz is described. However, the calibration uncertainty due to the dependence of the probe sensitivity on polarization, frequency, dielectric parameters of the surrounding media and spatial resolution have only been marginally addressed. In this paper these issues are analyzed and a calibration procedure enabling accurate calibration of the probes for a broad frequency range in two lossy dielectric liquids is described. A flexible setup has been chosen in order to study ways of minimizing the uncertainty of dosimetric assessments in the frequency range of mobile communications.

II. E-FIELD PROBE DESIGN AND MEASUREMENT

ERRORS

The main requirements for E-field probes in any type of surrounding medium are:

- high degree of isotropy in various media;
- high sensitivity and linear response over a broad frequency range;
- high spatial resolution (small tip size); and
- low interaction with the measured field.

E-field probes with isotropic response can be achieved by the orthogonal positioning of three sensors that are sensitive to one E-field component each. Short dipoles or small E-field-sensitive crystals have these characteristics. In miniaturized E-field probes small dipoles with diode rectifiers are mainly used, because they offer the greatest sensitivity and have a linear response over a wide frequency range. A design with a triangular core was chosen for the new E-field probe. This design provides a small outline and shows a high degree of symmetry (Figure 1). The sensors themselves consist of three small dipoles (3 mm in length) directly loaded with a Schottky diode and connected via resistive lines to the data acquisition electronics.

In the following, a number of design problems of these probe types are mentioned; some of them apply to other probe types as well. A more detailed description of the probes is given in [2].

1.) *Secondary modes of reception:* Resistive lines are used to transmit the signal from the rectifier diodes to the evaluation electronics. The interaction of these lines with the field should be minimal. Nevertheless, RF signals can be picked up by the lines and detected and rectified by the diodes. These secondary reception modes appear mainly at lower frequencies, where the impedance of the dipole and the diodes is very high and can produce disturbed directivity characteristics. Special filtering techniques or high

Abstract—A broadband calibration procedure for E-field probes that minimizes the overall uncertainties inherent in E-field measurements in lossy dielectric liquids has been developed. The analysis of the calibration requirements shows that probes that are symmetrical with respect to their axes greatly facilitate accurate calibration, since the calibration procedure can be divided into several discrete steps. Such a procedure is presented and analyzed with respect to its uncertainties. Absolute calibration is performed at three frequencies (450 MHz, 900 MHz and 1.8 GHz) and in different tissue-simulating liquids. The parameters obtained are verified by numerical simulations of the probe in the surrounding media. Such simulations allow the assessment of some of the calibration parameters with sufficient accuracy in cases where the experimental determination would be too tedious and time-consuming.

I. INTRODUCTION

The interaction of high-frequency electromagnetic fields with biological matter has been the object of growing interest for several years. Miniature E-field probes have been developed to determine experimentally the induced electric field in actual tissue or tissue-simulating liquids. In view of the phenomenal growth of the mobile communications market, the telecommunications industry has lately recognized the need to test its mobile telephones for compliance with today's safety limits. The key value for dosimetric assessments in general and compliance tests in particular is the maximum tolerable absorbed power per tissue mass in mW/g, known as the specific absorption rate (SAR). The local SAR can be determined experimentally by measuring either the induced electrical field strength or the temperature rise in tissue.

where σ is the conductivity, ρ is the mass density and c is the specific heat of the tissue at the site of measurement. Since measurements using thermal probes do not provide an adequate degree of efficiency and sensitivity for compliance-testing of consumer products, the research up until today has been focused on small isotropic E-field probes. The original design of a miniaturized isotropic E-field probe for use in tissue-simulating liquids goes back to Bassen et al. [1] Recently the authors presented a new probe design [2] with significantly improved performance. In view of the significance of, and the difficulties involved in, accurate calibration, surprisingly little has been

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III. CALIBRATION REQUIREMENTS

The three output signals from an isotropic E-field probe with three orthogonally positioned sensors must be evaluated to give a reading that corresponds to the SAR at the measurement site in the absence of the probe. The relation between the field and the sensor signals depends on various factors:

- design and construction materials of the probe;
- electrical properties of the surrounding media;
- direction and polarization of the field;
- field gradient at the measurement site;
- RF characteristics of the antenna, the rectifying element and the transmission line;
- higher order modes or different reception modes in the probe;
- sensitivity of the rectifier; and
- characteristics of the evaluation circuit for the rectified signals.

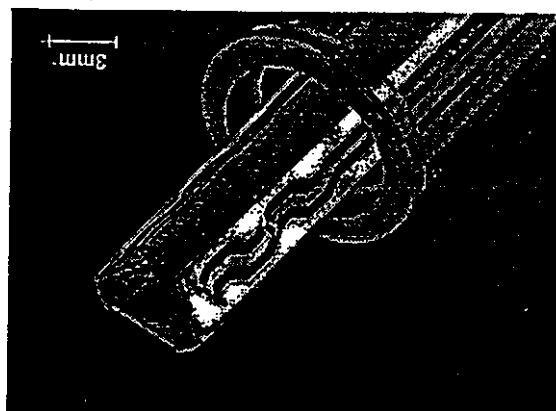
Each calibration essentially attempts to describe these effects quantitatively, so that correct SAR values can be obtained under various measurement conditions. Furthermore, it is important to know the absolute uncertainty and the validity range of the calibration. To keep the number of calibration parameters and calibration measurements low, it is crucial to separate the above-listed influences and quantify them individually. An effective way must be found to reduce the effect of any possible further errors that can arise under various measurement conditions. The probe design is a deciding factor in this regard. For our dosimetric probes, a three-step calibration process has proven to be the most effective approach:

$$(2) \quad |E_z| = \sum_{i=1}^3 f_i(V_i) \eta_i \gamma_i$$

a) $f_i(V_i)$: The rectified signal of each sensor (V_i) is linearized. The linearization function depends on the characteristics of the rectifier and the evaluation circuit. It can be described as a function of the magnitude of the rectified signal and can be assessed easily by a power sweep of the exciting field. When the rectifying elements and evaluation channels are identical, the same function $f(f_i(V_i) = f(V_i))$ can be used for all sensors. In the case of amplitude-modulated signals, the timing characteristics of the evaluation circuit must also be taken into account, unless the signal stays within the "square law" region of the detector element, or the evaluation is rapid enough to keep pace with the modulation. For pulsed signals with a known crest factor, a simple correction formula can be given; for arbitrary modulations, however, a more sophisticated signal analysis is necessary.

b) η_i : These factors describe the absolute sensitivities of the probe sensors ($\mu V/(V/m)^2$) in air for which γ_i is equal to one. They depend on the probe construction materials, the sensor positioning and the RF characteristics of the sensor components. If detector diodes are used as rectifying elements, the parasitic capacitance, which is generally not precisely specified, influences the RF behavior.

Fig. 1. Tip of the E-field probe. The tip encapsulation has been removed. One 3 mm long dipole and the diode can be seen. In the center of the core is the opening for a built-in optical proximity sensor.



ohmic lines can reduce this effect. [2]

2.) *Influence of the probe materials on the field*: Any dielectric material around electric dipoles can have an effect on the local signal strength inside the probe. It is obvious from the construction of these probes that the influence on E-field components normal to the probe axis will be different from that on E-field component parallel to the probe axis. Furthermore, this difference in sensitivity depends on the surrounding medium. This results in poor isotropy in planes along the probe axis. In [2], several methods are presented to compensate for these effects. In any case the directivity characteristic of the probe will be different in different media. This has to be taken into account when calibrating the probe in a specific medium.

3.) *Influence of the probe on nonhomogeneous fields*: The disturbance caused by the probe on nonhomogeneous fields depends both on the geometrical and material properties of the probe and on the nature of the field itself. The influence of these effects must be investigated in each case. Errors in SAR readings can occur when using the probe in the immediate vicinity of material discontinuities – for instance, when the probe approaches the surface of a shell phantom (see also Figures 6 to 9). By performing measurements at different distances from the surface and extrapolating to the surface, corrected SAR values for the vicinity of the surface can be obtained.

4.) *Spatial resolution*: Another source of error in non-homogeneous fields arises from the spacing between the dipole centers in the probe. Since each field component is measured at a slightly different location, discrepancies are to be expected when the field's magnitude or direction varies greatly within the probe's dimensions. By turning the probe along its long axis, the measurement locations of the three sensors shift and a further isotropy error will occur.

Therefore, a calibration setup that minimizes these errors must be carefully chosen.

To calibrate the probe in air, a well-defined measurement volume with an absolutely known and largely homogeneous electrical field is necessary. The field strength can be measured with a standard calibrated probe, if available; otherwise, it must be determined from power measurements. Several methods are used to produce such fields:

a) Far field of standard radiators: These calibrations are

IV. CALIBRATION IN AIR

At higher frequencies and in lossy media, the fields have high gradients. If the gradient is significant within the probe's dimensions, a calibration reference point in the probe must be defined. The field gradient will result in further isotropy errors depending on the probe's alignment with respect to the direction of the field gradient. For the best calibration results, the calibration setup should be as close as possible to the actual measuring situation.

The validity of these assumptions depends largely on the probe's design. Measurements and simulations of our probes have established the feasibility of this calibration procedure. However, it is necessary to reassess the deviation from isotropy in liquid, since it may differ from air. (see Section II).

- The construction differences (manufacturing tolerances) between probes of the same type are small.
- The validity of these assumptions depends largely on the probe's design. Measurements and simulations of our probes have established the feasibility of this calibration procedure. However, it is necessary to reassess the deviation from isotropy in liquid, since it may differ from air.
- The construction differences (manufacturing tolerances) between probes of the same type are small.
- The condition can be regarded more leniently.
- The surrounding medium. In symmetrical probes this condition can be regarded more leniently.
- The local E-field distribution in the area of the sensors inside the probe only depends in magnitude on the surrounding medium. In symmetrical probes this condition can be regarded more leniently.
- The variation of the dipole impedance caused by the surrounding medium is the same for all sensors.
- The local E-field distribution in the area of the sensors inside the probe only depends in magnitude on the surrounding medium. In symmetrical probes this condition can be regarded more leniently.

The separation of the calibration factor in a probe and the "conversion factor".

These factors describe the ratio of the sensitivity of the probe sensors in different media to their sensitivity in air. These usually depend both on the surrounding material and the frequency and on the constructional materials and the design of the probe. They will be identical for each probe of the same type. In the case of symmetrical sensors (time-consuming) this implies that the (time-consuming) assessment of these calibration factors (see Sections V and VI) need to be done only once for each probe type, and not for each individual probe. γ will hereafter be called the "conversion factor".

Therefore, the factors γ_i will be different for each sensor, even if the sensors are positioned in a symmetrical fashion. These factors can be assessed by standard probe calibration procedures (see Section IV). All error sources (isotropy, frequency linearity) must be investigated during this calibration in order to assess the calibration factors for an average measurement situation and to evaluate the error and validity range of the calibration. For broadband and E-field probes, the calibration factors are independent of the frequency over a wide range (2 to 3 decades) and can thus be considered to be constants.

c) TEM cells produce a homogeneous TEM wave in a limited volume ($\ll$ wavelength). The highest usable frequency is determined by the existence of higher-order propagation modes (200 MHz to 1.5 GHz, depending on the cell size). The power can be measured at the output of the cell. The accuracy is limited by cell impedance variations due to constructional inaccuracies. The discontinuities in the construction (edges, access openings) produce field deviations

b) Near field of radiators: In the near field, it is not easy to determine the absolute field strength. However, the direction of the field vector is often determined by simple symmetry considerations. These fields can be used to measure the relative directivity of the probe when the field gradient is small compared to the probe dimensions.

done in free space or in anechoic chambers. The open measurement area permits the positioning of the probe easily at any angle towards the field. The radiated power can be measured with high accuracy. Errors in the determination of the antenna gain and reflections limit the absolute accuracy of this calibration method to approximately ± 0.5 dB.

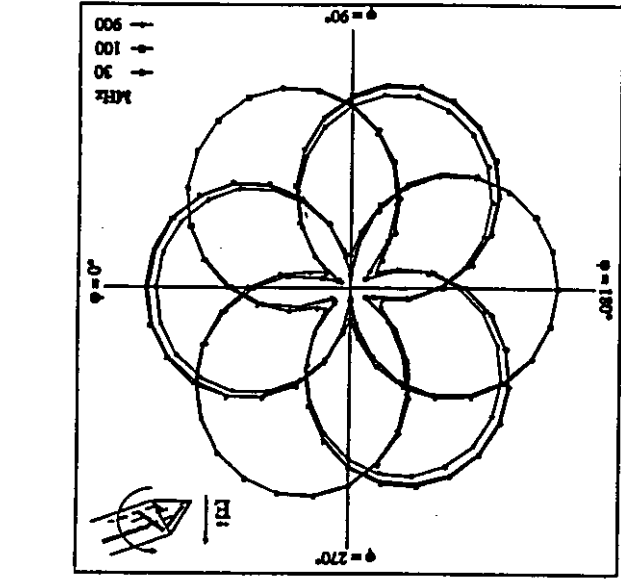


Fig. 3. Receiving pattern of the three orthogonally arranged dipoles after calibration in air. E-field is normal to the probe axis.

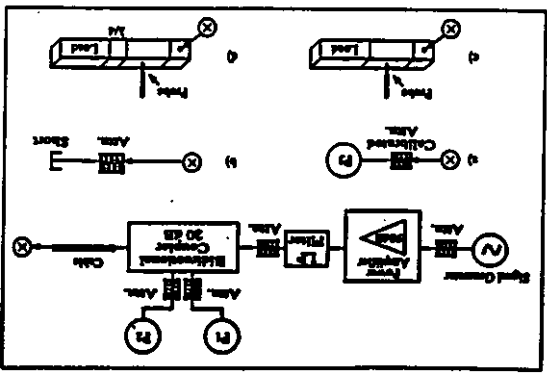


Fig. 2. Setup for calibration in waveguides (air). Measurements a and b to calibrate the power meters P_1 and P_2 . P_3 is a high-precision meter. Probe measurements c and d with different distances to load.

which allow the computation of the field inside the dielectric material analytically or by numerical simulations. One way would be a dielectric slab in a rectangular waveguide. Although the induced fields are well defined and can be determined easily if the emergence of spurious higher modes can be sufficiently suppressed, the setup is very narrow-banded.

Another setup used in [4] is the simulation of a dielectric half-space, which is exposed to a $\lambda/2$ dipole parallel aligned to the surface of this half-space (Figure 4). This configuration can be accurately simulated by using numerical techniques, since the SAR on the axis is predominantly proportional to the square of the antenna feedpoint current and not to the output power. However, experimentally, the feedpoint current can be assessed only with fairly large uncertainties of no better than $\pm 10\%$.

Nevertheless this setup was chosen because:

- It is easy to build up and to handle.
- It provides much greater flexibility since a broad frequency range can be covered by the same setup.
- It is a good representation of the test situation implemented for dosimetric assessments of mobile communications devices [5].
- In lossy dielectric liquids, the local SAR values can be experimentally measured by small thermal probes according to equation (1) at high power levels.

The half-space is simulated by an acrylic glass box ($600 \times 300 \times 200 \text{ mm}^3$) filled with the lossy dielectric liquid. The thickness of the acrylic glass box phantom is 4 mm. The dipoles are placed parallel to the dielectric surface at distances that are small compared to the dimensions of the box and to the distance from the floor. The floor is lined with absorbers.

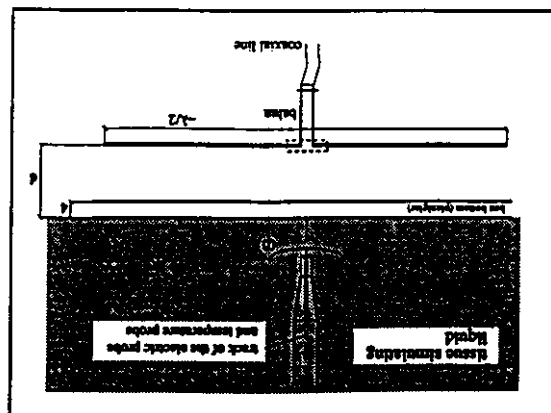
The dipole used at 450 MHz is a Stoddard dipole 310 mm long, and at 900 MHz a high-precision dipole 147 mm long and 3.6 mm in diameter is used. In both cases, the dipoles are driven by an HP8656B generator and a broadband RF power amplifier (Kalmus Model 717C, 100 W output power). A bidirectional coupler HP775D monitors the forward and reflected power. The 1.8 GHz dipole is 73.5 mm in length and has a diameter of 2.25 mm. Losses along the coupler and the lines are taken into account.

In the following, the conversion factors γ for brain-simulating tissues at 450 MHz, 900 MHz and 1800 MHz are determined.

B. Brain Simulating Liquids

The simulating liquids for brain tissue at 450 MHz and 900 MHz consist of sugar, water, NaCl and Hydroxyethyl-cellulosis (HEC). [6] For brain tissue at 1.8 GHz, two different liquids were used. The first was based on a simple sugar-water solution without any salt (free ions). Nevertheless, the conductivity of such a solution was still higher than most recent data for living tissue [7] would suggest (Table I). At frequencies higher than 1 GHz, the bound sugar-water complexes begin to determine the conductivity level of the liquid. Therefore, in a second approach, sugar was replaced by butyldiol (2-(2-butoxyethoxy)ethanolbutyl).

Fig. 4. Experimental setup. On the top is the Plexiglas box filled with the simulating liquid. At the bottom is the dipole. The temperature probes and the E-field probe are positioned directly above the dipole feedpoint.



from the theoretical TEM mode. An absolute accuracy of $\pm 0.4 \text{ dB}$ is possible.

(d) GTEM cells have no discontinuities and can be used from DC to several GHz. The calibration volume can have dimensions of several wavelengths. The reflections from the built-in absorber and load produce standing waves, which limit the absolute accuracy of GTEM cells to ± 1 to $\pm 3 \text{ dB}$.

(e) Waveguides produce well-defined fields in small volumes and a limited frequency band. With high-precision components (loads, lines, adaptors to coaxial lines) and error compensation, the field can be determined to be within $\pm 2\%$. However, the influence of the probe itself on the field must be carefully investigated.

For the absolute probe calibration in air, we used methods c) and e). At frequencies over 1 GHz we measured in standard waveguides R22 and R26, with a setup according to Figure 2. The probe is rotated around its axis with a positioning accuracy at the probe tip of better than $\pm 0.1 \text{ mm}$. Absolute accuracy of the calibration is given for an average in the directivity and lies within $\pm 5\%$ (The linearity over different frequencies and waveguides is better than $\pm 2\%$). At frequencies below 1 GHz, a TEM cell in 110 was used for calibration (Figure 3).

The agreement in absolute value with the measurements in the waveguides is better than could be expected from the cell data (within $\pm 3\%$). Waveguide measurements at 900 MHz will be performed to confirm this agreement. As the directivity for all rotational angles of the probe cannot be determined in waveguides, a near-field exposure situation was used. For higher frequencies, the center point over an open waveguide was chosen as the measurement site and, for lower frequencies, the field in the symmetry plane of highly symmetrical standard dipoles.

V. CALIBRATION IN LOSSY DIELECTRIC LIQUIDS

A. Setup

To determine the conversion factor γ , a well-defined SAR distribution inside the dielectric material for which the probe must be calibrated is needed. Setups are preferred

TABLE I
DIELECTRIC PROPERTIES OF BRAIN TISSUE-SIMULATING LIQUIDS AT THE TESTED FREQUENCIES. AT 1.8 GHz, TWO LIQUIDS WERE USED: SUGAR-WATER SOLUTION (A) AND BUTHYLDIGOL-WATER SOLUTION (B).

Frequency [MHz]	ϵ'	σ [mho/m]
450	47.0 $\pm 5\%$	0.43 $\pm 6\%$
900	40.0 $\pm 5\%$	0.87 $\pm 6\%$
1800A	40.5 $\pm 5\%$	1.75 $\pm 6\%$
1800B	41.5 $\pm 5\%$	1.25 $\pm 6\%$

which, when dissolved in water, shows smaller conductivity values. At the same ϵ' value, the conductivity could be reduced from 1.75 to 1.25 mho/m. The electrical parameters were measured by an open coaxial method using the HP 85070A Dielectric Probe Kit. To verify the open coaxial method, we determined the electrical parameters using the slotted-line method. The agreement was within 4%. Table I gives an overview. The temperature dependence of the liquid's parameter was also checked. In the temperature range between 15°C and 30°C, a change of 5% was measured, which lies within the uncertainty of the permittivity measurement method.

The specific thermal constant c was determined using a simple calorimetric procedure with an accuracy of better than $\pm 4\%$. The specific density ρ and c depend mainly on the ratio between sugar and water. For brain tissue-simulating liquids, c was determined to be $2.85 \text{ J/K/g} \pm 4\%$ with a specific density (ρ) of $1.30 \text{ g/cm}^3 \pm 1\%$. Comparison of these values for c with data from literature shows considerable agreement. Gucker *et al.* measured 2.90 J/K/g for a similar aqueous sucrose solution. [8] The value for the brain tissue-simulating liquid which uses the sugar substitute Buthyldigol is 3.58 J/K/g ($\rho = 0.98 \text{ g/cm}^3 \pm 1\%$).

C. Temperature Probe

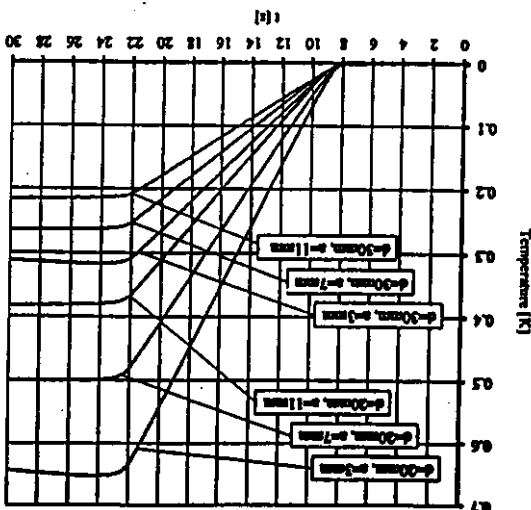
The measurement of the local SAR by temperature probes has the advantage that temperature is a scalar value. Small sensors can therefore be easily produced. Immunity of the temperature probes towards the HF fields must be guaranteed and can be achieved by optical probes or thermistor probes with high resistive lines. [9] The limited temperature sensitivity of these sensors can be overcome by applying high power.

In this study, the nonmetallic temperature measurement

TABLE II
CONVERSION FACTOR γ , WHICH DESCRIBES THE INCREASE OF SENSITIVITY IN BRAIN TISSUE-SIMULATING LIQUIDS AT THE TESTED FREQUENCIES.

Frequency [MHz]	ϵ'	σ [mho/m]	γ
450	47.0	0.43	6.7 $\pm 10\%$
900	40.0	0.87	6.0 $\pm 10\%$
1800A	40.5	1.65	4.8 $\pm 10\%$
1800B	41.0	1.25	4.8 $\pm 10\%$

Fig. 5. Temperature increase measured during RF exposure to a 900 MHz field. The power input was 43 dBm. d = dipole distance from the stimulating liquid; a = sensor distance from the acrylic glass bottom.



system (SPAG DASY2) was used to measure the temperature increase. The probe is based on an NTC temperature sensor connected to four resistive lines. [10] The noise level of this system is about 100 times less than that of the two comparable optical devices on the market ($\pm 0.001^\circ\text{C}$ averaged over 0.1 s). The noise level for temperature rise measurement over a period of 10 s was found to be better than $\pm 0.1 \text{ mK/s}$. At these high frequencies (450 MHz - 1.8 GHz) the absorption is very local - i.e., close to the feedpoint of the dipole and rapidly decreasing the further it penetrates the tissue. This causes strong temperature gradients inside the liquid. Thus, thermodynamic dissipation processes, such as convection, had to be monitored. The RF power was usually on for about 14 seconds. The corresponding linear temperature increase was evaluated by least-square. After every exposure period, the liquid was stirred until a thermodynamic equilibrium state was reached again before the RF power could be switched on again. The temperature increase in the liquid due to exposure to a 900 MHz field at two distances from the body is shown in Figure 5. The effects of convection were assessed by evaluating different time intervals and were found to be negligible within the first 10 s for sugar-water solution. The solution based on Buthyldigol had considerably lower viscosity, so that the evaluation time had to be reduced to 5 s.

A robot positioned the temperature probe in the liquid by moving it from the top, like the E-field probes, towards the bottom of the box. The disturbance of the probe holder has proven to be negligible.

D. Results

The conversion factor γ was determined by comparing the SAR values measured by the temperature probe and by the E-field probe. The measurement points were located on a line normal to the Plexiglas bottom above the dipole

The accuracy of the conversion factor γ is mainly determined by the uncertainties in determining the correct electromagnetic and thermal properties of the tissue-simulating liquid. Using the "slot line" and "open coaxial" methods to determine the conductivity of the liquid introduces an uncertainty of about $\pm 6\%$. The specific heat of the liquid

the various tissues are summarized in Table II. The results for procedure considering all measured values. The results for source from the body and at different frequencies (Figures 6 to 9). The conversion factor was assessed by a least-square

Fig. 7. SAR assessed by E-field (small empty symbols) and temperature measurement (big full symbols) at 900 MHz in brain-simulating liquid ($\epsilon_r = 40.0$ and $\sigma = 0.67$ mho/m). The SAR was normalized on 1 Watt input power. The dipole distances from the body were 20 mm, 30 mm and 50 mm. The conversion factor γ was determined to $6.0 \pm 10\%$.

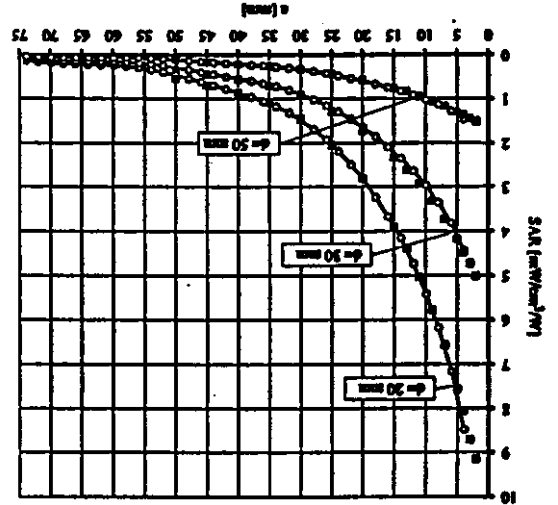
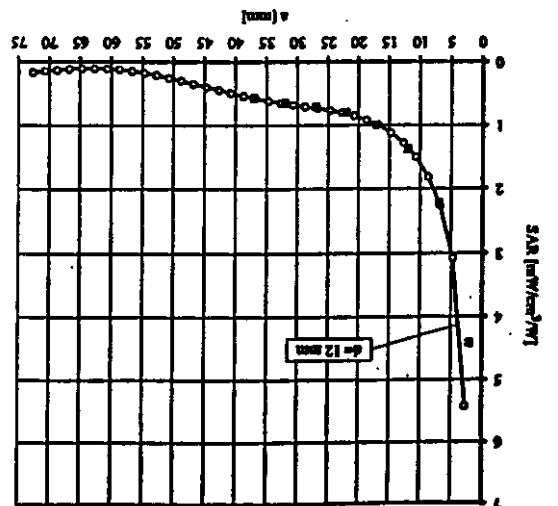


Fig. 6. SAR assessed by E-field (small empty symbols) and temperature measurement (big full symbols) at 450 MHz in brain-simulating liquid ($\epsilon_r = 47.0$ and $\sigma = 0.43$ mho/m). The SAR was normalized on 1 Watt input power. The frequency was set to 450 MHz. The dipole distance from the body was 12 mm. The conversion factor γ was determined to $6.7 \pm 10\%$.



Three objectives led us to use numerical techniques to simulate the probe embedded in lossy dielectric materials: 1) to study methods to improve the isotropy of the probes [2]; 2) to assess the spatial resolution; and 3) to determine the conversion factor γ computationally, since numerical

can be assessed to an accuracy of about $\pm 4\%$. The E-field probe yields another $\pm 3\%$. Adding the uncertainty of the positioning of the E-field probe ($\pm 1\%$), of the temperature probe ($\pm 2\%$), and of the power meters ($\pm 1\%$) leads to a total uncertainty of less than $\pm 10\%$.

Fig. 9. SAR assessed by E-field (small empty symbols) and temperature measurement (big full symbols) at 1.8 GHz in brain-simulating liquid ($\epsilon_r = 41.0$ and $\sigma = 1.25$ mho/m). The SAR was normalized on 1 Watt input power. The dipole distances from the body were 10 mm, 20 mm and 30 mm. The conversion factor γ was determined to $4.8 \pm 10\%$.

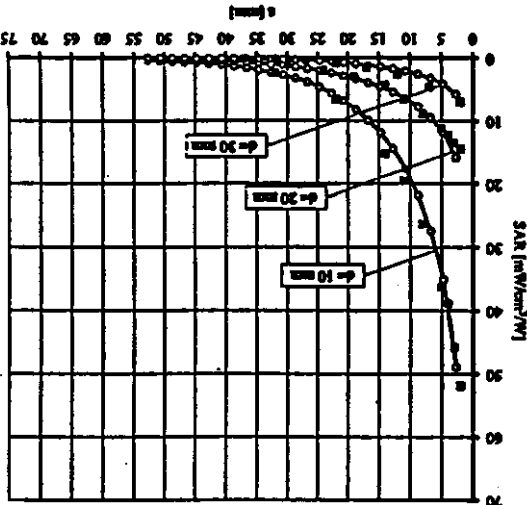
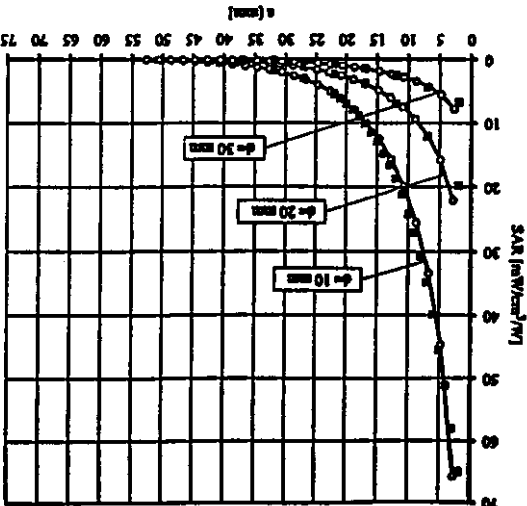


Fig. 8. SAR assessed by E-field (small empty symbols) and temperature measurement (big full symbols) at 1.8 GHz in brain-simulating liquid ($\epsilon_r = 40.5$ and $\sigma = 1.75$ mho/m). The SAR was normalized on 1 Watt input power. The dipole distances from the body were 10 mm, 20 mm and 30 mm. The conversion factor γ was determined to $4.8 \pm 10\%$.



voxels were needed to model the whole computational domain and to use a minimal number of expansion functions, at the corners of the probe. In order to minimize these errors and to use a minimal number of expansion functions, maximum errors (<10%) appeared on the matching points two domains and 9 multipole expansions. As expected, the required about 550 matching points at the boundary of the homogeneous model of the probe. In MMP, the modeling the probe tip. MMP could only be used for this simple proven to be long enough to study the fields induced in probe. The length of the cylinder is 15 mm, which has a simple homogeneous, lossless cylinder 6.8 mm in diameter with a relative permittivity of 2.54. This corresponds to the electrical properties of the microwave material utilized (STYCAST 0005) to build the core of the probe. The simplest numerical representation of the probe

a) The simplest numerical representation of the probe

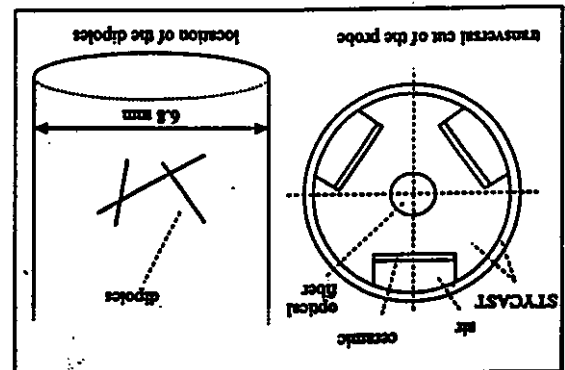
have been compared: Different discretizations with increasing complexity the location of the dipoles inside the probe is shown in Fig. 10. A transversal cut of the probe and a perspective view with different discretizations of the E-field probe were chosen. A ing on the electrical parameters of the surrounding media, To study the field distribution inside the probe depend-

A. Modeling of the probe

The first one is the 3D MMP software package developed at the Swiss Federal Institute of Technology (ETH). It is a frequency domain boundary technique suited for 2D and 3D scattering problems within piecewise linear, homogeneous and isotropic domains. Details are given in [11] and [12]. The second software package, "MAFLA", was developed at the Technische Hochschule Darmstadt (THD), Germany. The method used is based on the finite integration technique (FIT) and is very similar to an FDTD approach. Details are given in [13] and [14].

techniques are less tedious than the experimental approach. To obtain a deeper insight into the behavior of the convolution factor, two numerical packages based on two different techniques were used. This had the advantage of the possible cross-validation of the results obtained by both techniques, each of which has its strengths in different areas.

Fig. 10. Computer simulation model: transversal cut of the probe and location of the dipoles.



As the reference value, the E-field at the location of the dipole center in the absence of the probes was chosen.

$$\gamma = \frac{\sum_{i=1}^3 \left(\int_{dipole} E_{ds}(in\ air) \right)^2}{\sum_{i=1}^3 \left(\int_{dipole} E_{ds}(in\ tissue) \right)^2} \quad (3)$$

In all the models the dipoles were not simulated. The conversion factor can be calculated by integrating the electric field at the location of the dipoles, firstly with biological tissue surrounding the structure and then with air around it:

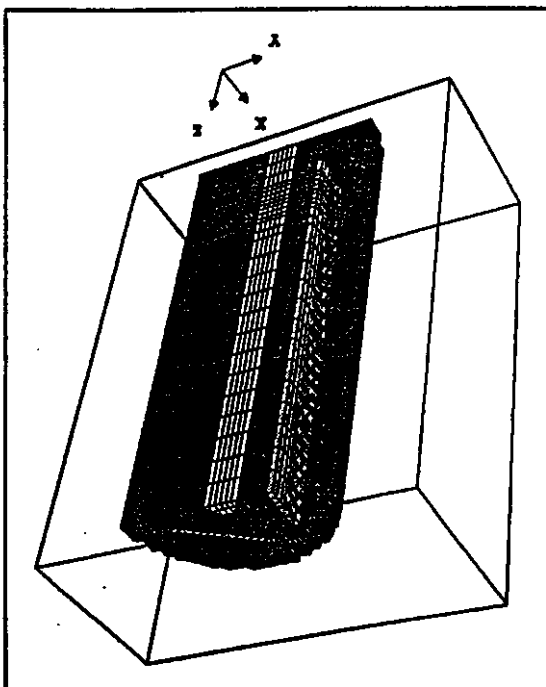
d) In the most complex model, three ceramic sheets on which the dipoles and lines are printed were simulated as well (Figure 11). This leads to a discretization with 210,000 voxels, about 37,000 of which were needed for the probe itself.

c) Additional details were incorporated in a further model by the modelling of the three air holes (Figure 10). smaller homogeneous cylinder 1 mm in diameter with a relative permittivity of 5 in the center of the STYCAST

b) A more complex model simulated the optical fiber in the center of the core. The fiber was discretized as a smaller homogeneous cylinder 1 mm in diameter with a reflected waves was assumed to be less than 3%.

main within MAFLA, about 5,000 of which were needed for the probe itself. Problems occur at the outer boundaries when using open-boundary conditions and assuming the whole computational domain to be of a lossy material, as in the case of biological tissue. Nevertheless, in choosing a long computational domain in the direction of the wave propagation vector and in considering that the attenuation over one wavelength is very slight, the influence of possible

Fig. 11. Computer simulation model: complex model of the probe for the MAFLA simulation tool.



B. Results of the Simulations

Figure 1 is a line graph showing the relationship between Relative Permeability (Y-axis, ranging from 5 to 50) and Conversion Factor T (X-axis, ranging from 0 to 8). The graph compares five different models:

- Stone and air holes
- Stone, air holes, ceramic sheet
- homogeneous model
- optical fibers included
- optical fibers included

The graph illustrates that relative permeability generally decreases as the conversion factor T increases for all models. The 'Stone and air holes' model consistently shows the highest relative permeability, while the 'optical fibers included' models show the lowest relative permeability across the range of conversion factors.

Graph showing Relative Permeability (Y-axis, 20 to 50) versus Conversion Factor γ (X-axis, 0 to 8). Two curves are plotted for different values of σ :

- $\sigma = 0$ (Upper curve)
- $\sigma = 0.25$ (Lower curve)

Both curves show a sharp increase in permeability as γ increases beyond 5.

Fig. 14. Experimentally assessed conversion factor for brain tissue-simulating liquid in comparison with the values obtained from numerical simulation for homogeneous (empty symbols) and non-homogeneous (filled symbols) modellings of the probe.

Figure 7 is a line graph comparing the frequency response of the proposed model with the calculated frequency response of the model. The y-axis represents Frequency [Hz] from 0 to 2000, and the x-axis represents Conversion Factor from 0 to 8. Three data series are plotted: 'calculated frequency response' (top line), 'proposed model' (middle line), and 'reference' (bottom line). All three series show a decreasing trend as the conversion factor increases.

Conversion Factor	calculated frequency response [Hz]	proposed model [Hz]	reference [Hz]
0	~1800	~1700	~1600
1	~1600	~1500	~1400
2	~1400	~1300	~1200
3	~1200	~1100	~1000
4	~1000	~900	~800
5	~800	~700	~600
6	~600	~500	~400
7	~400	~300	~200
8	~200	~100	~0

VII. CONCLUSIONS

A procedure has been presented that allows an absolute calibration of the probes for dosimetric assessments with an accuracy of better than $\pm 10\%$. The chosen approach has the advantage that the calibration setup closely corresponds to that of the actual dosimetric assessments performed with the scanner described in [5]. Thus, further considerations with regard to polarization are not required. If such studies are needed, the techniques described in [5] can be used. Numerical techniques have proven to be adequate to assess the conversion factor γ if a precision of only $\pm 20\%$ is sufficient for this probe. For other probe designs, the uncertainties of the numerically determined conversion factors might be considerably larger.

VIII. ACKNOWLEDGMENTS

We gratefully acknowledge the help of Mr. Oliver Egger, Mrs. Katja Poković and Mr. Jeroen de Keijzer for their support in this study.

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Appendix 8

pages 1 - 7

DIPOLE VALIDATION KIT

DASY

Dipole Validation Kit

Type: D900V2

Serial: 003

Manufactured: August 1995
Calibrated: August 1998

1. Measurement Conditions

The measurements were performed in the flat section of the new generic twin phantom (shell thickness 2mm) filled with brain simulating sugar solution of the following electrical parameters at 900 MHz:

Relative Dielectricity	42.8	± 5%
Conductivity	0.85 mho/m	± 5%

The DASV3 System (Software version 1.0a) with a dosimetric E-field probe ET3DV4 (SN:1302, Conversion factor 5.5) was used for the measurements.

The dipole was mounted on the small tripod so that the dipole feedpoint was positioned below the centre marking of the flat phantom section and the dipole was oriented parallel to the body axis (the long side of the phantom). The standard measuring distance was 15mm from dipole centre to the solution surface. The included distance holder was used during measurements for accurate distance positioning.

The coarse grid with a grid spacing of 15mm was aligned with the dipole. The 5x5x7 fine cube was chosen for cube integration. Probe isotropy errors were cancelled by measuring the SAR with normal and 90° turned probe orientations and averaging. The dipole input power (forward power) was 250mW ± 3 %. The results are normalised to 1W input power.

2. SAR Measurement

Standard SAR-measurements were performed with the phantom according to the measurement conditions described in section 1. The results have been normalised to a dipole input power of 1W (forward power). The resulting averaged SAR-values are:

averaged over 1 cm³ (1 g) of tissue: 9.36 mW/g

averaged over 10 cm³ (10 g) of tissue: 6.16 mW/g

Note: If the liquid parameters for validation are slightly different from the ones used for initial calibration, the SAR-values will be different as well. The estimated sensitivities of SAR-values and penetration depths to the liquid parameters are listed in the DASV Application Note 4: 'SAR Sensitivities'.

3. Dipole Impedance and return loss

The impedance was measured at the SMA-connector with a network analyser and numerically transformed to the dipole feedpoint. The transformation parameters from the SMA-connector to the dipole feedpoint are:

Electrical delay:	1.416 ns	(one direction)
Transmission factor:	0.993	(voltage transmission, one direction)

The dipole was positioned at the flat phantom sections according to section 1 and the distance holder was in place during impedance measurements.

Feedpoint impedance at 900 MHz: $\text{Re}\{Z\} = 49.9 \Omega$

$\text{Im}\{Z\} = 3.4 \Omega$

Return Loss at 900 MHz: -29.6 dB

4. Handling

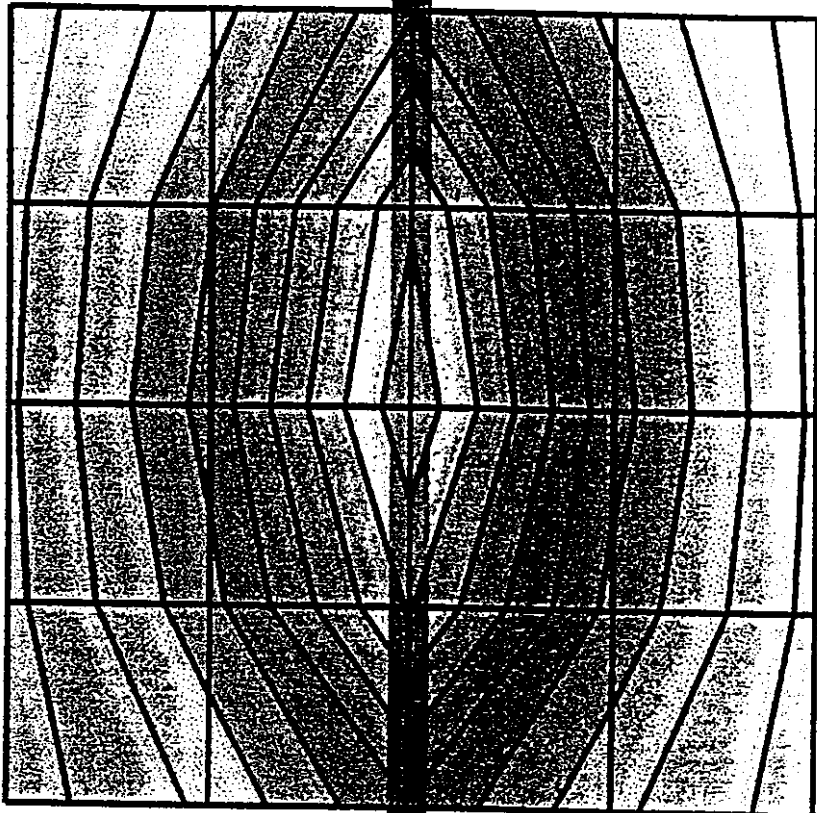
The dipole is made of standard semirigid coaxial cable. The centre conductor of the feeding line is directly connected to the second arm of the dipole. The antenna is therefore short-circuited for DC-signals.

Do not apply excessive force to the dipole arms, because they might bend. If the dipole arms have to be bent back, take care to release stress to the soldered connections near the feedpoint; they might come off.

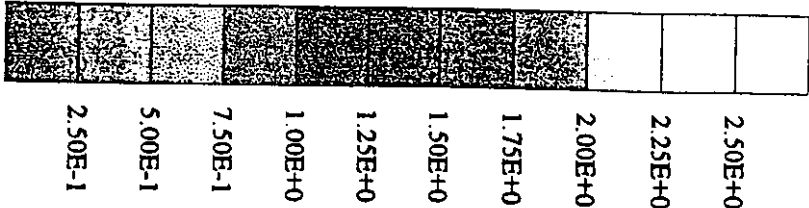
After prolonged use with 100W radiated power, only a slight warming of the dipole near the feedpoint can be measured.

ation Dipole D900V2 SN:003, d = 15mm

y: 900 [MHz]; Antenna Input Power: 250 [mW]
[Twin Phantom; Flat Section; Grid Spacing: Dx = 20.0, Dy = 20.0, Dz = 10.0
T3DV5 - SN1302/DAE3; ConvF(5.50,5.50,5.50); Brain 900 MHz: $\sigma = 0.85$ [mho/m] $\epsilon_r = 42.8$ $\rho = 1.00$ [g/cm³]
): Peak: 3.56 [mW/g] ± 0.05 dB, SAR (1g): 2.34 [mW/g] ± 0.05 dB, SAR (10g): 1.54 [mW/g] ± 0.05 dB, (Worst-case extrapolation)
on depth: 13.1 (11.9, 14.6) [mm]
A: 0.00 dB



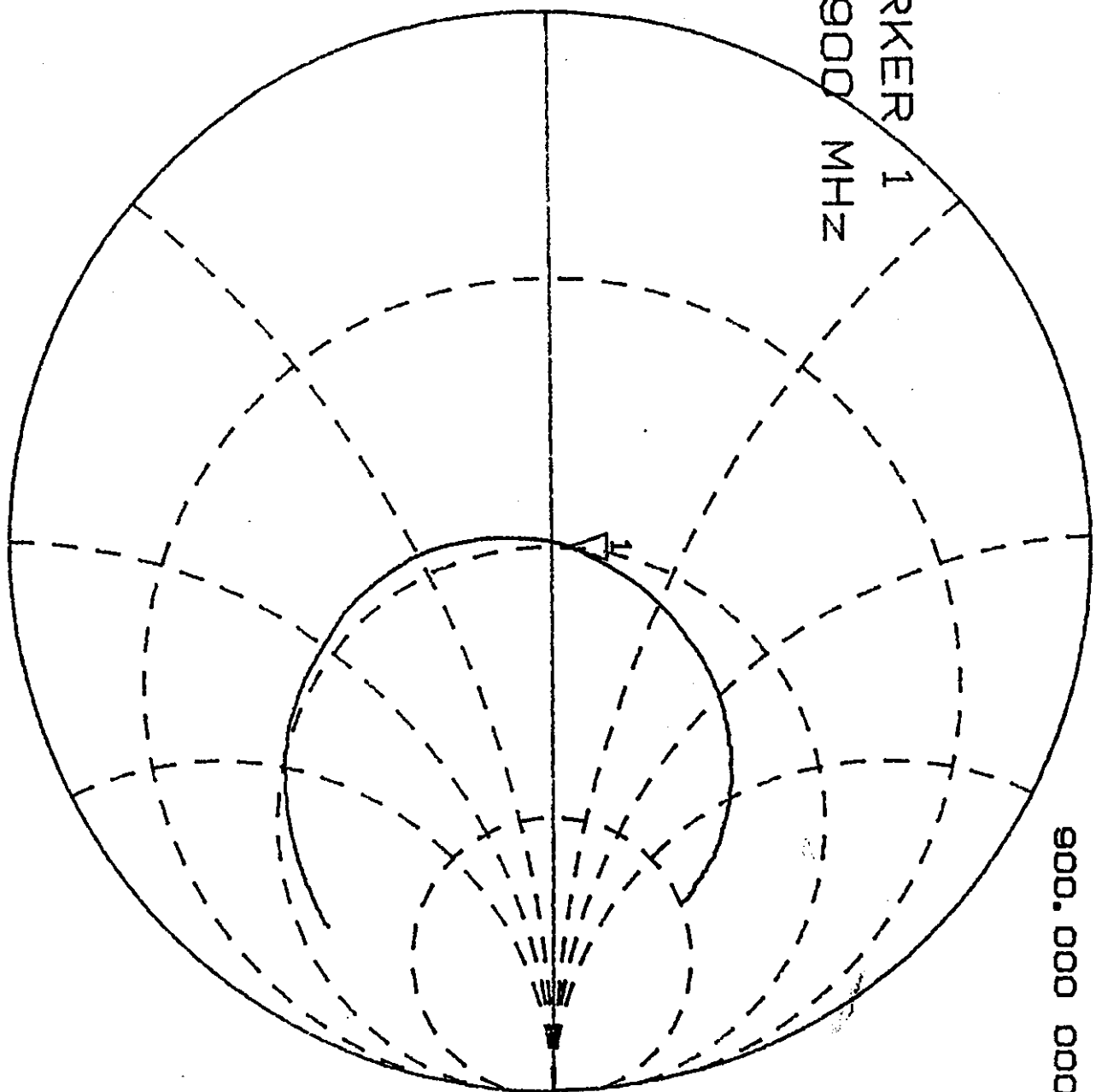
SAR_{Tα} [mW/g]



41 S11 988.9 mU 1. 49.986 Ω 3.3516 Ω 592.69 pF
900.000 000 MHz

31
31

MARKER 1
900 MHz



CENTER 900.000 000 MHz SPAN 400.000 000 MHz

11 S11 log MAG 5 dB/ REF 0 dB 11-29.564 dB

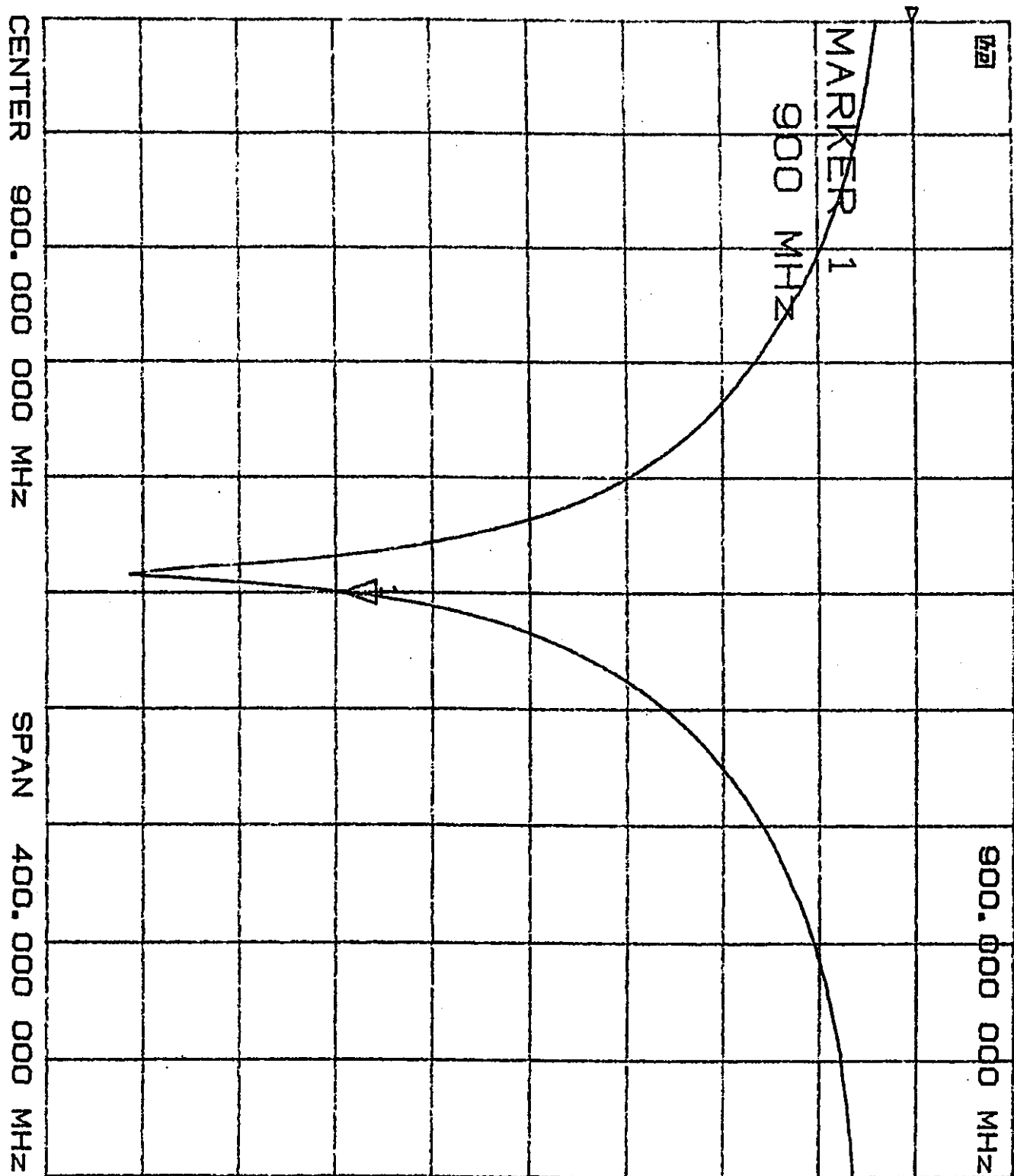
dB

900.000 000 MHz

or
31

MARKER 1

900 MHz



DASY3

Dipole Validation Kit

Type: D1800V2

Serial: 207

Manufactured: July 1997
Calibrated: August 1998

1. Measurement Conditions

The measurements were performed in the flat section of the new generic twin phantom (shell thickness 2mm) filled with brain simulating sugar solution of the following electrical parameters at 1800 MHz:

Relative Dielectricity	40.1	± 5%
Conductivity	1.65 mho/m	± 10%

The DASV3 System (Software version 3.0b) with a dosimetric E-field probe ET3DV4 (SN:1302, conversion factor 4.6) was used for the measurements.

The dipole feedpoint was positioned below the centre marking and oriented parallel to the body axis (the long side of the phantom). The standard measuring distance was 10mm from dipole centre to the solution surface. The included distance holder was used during measurements for accurate distance positioning.

The coarse grid with a grid spacing of 15mm was aligned with the dipole. The 5x5x7 fine cube was chosen for cube integration. Probe isotropy errors were cancelled by measuring the SAR with normal and 90° turned probe orientations and averaging. The dipole input power (forward power) was 250mW ± 3 %. The results are normalised to 1W input power.

2. SAR Measurement

Standard SAR-measurements were performed with the head phantom according to the measurement conditions described in section 1. The results (see figure) have been normalised to a dipole input power of 1W (forward power). The resulting averaged SAR-values are:

averaged over 1 cm ³ (1 g) of tissue:	37.1 mW/g
averaged over 10 cm ³ (10 g) of tissue:	18.5 mW/g

Note: If the liquid parameters for validation are slightly different from the ones used for initial calibration, the SAR-values will be different as well. The estimated sensitivities of SAR-values and penetration depths to the liquid parameters are listed in the DASV Application Note 4: 'SAR Sensitivities'.

3. Dipole Impedance and return loss

The impedance was measured at the SMA-connector with a network analyser and numerically transformed to the dipole feedpoint. The transformation parameters from the SMA-connector to the dipole feedpoint are:

Electrical delay:	1.236 ns	(one direction)
Transmission factor:	0.971	(voltage transmission, one direction)

The dipole was positioned at the flat phantom sections according to section 1 and the distance holder was in place during impedance measurements.

Feedpoint impedance at 1800 MHz: $\text{Re}\{Z\} = 49.9 \Omega$

$\text{Im}\{Z\} = -1.5 \Omega$

Return Loss at 1800 MHz - 36.0 dB

4. Handling

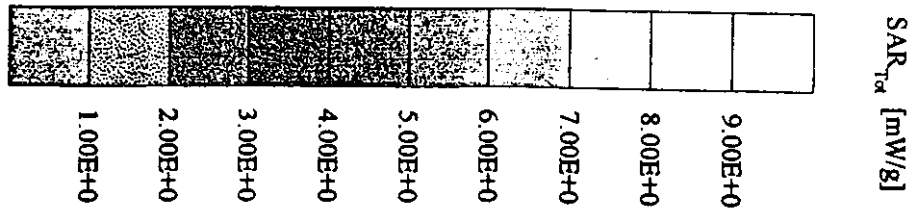
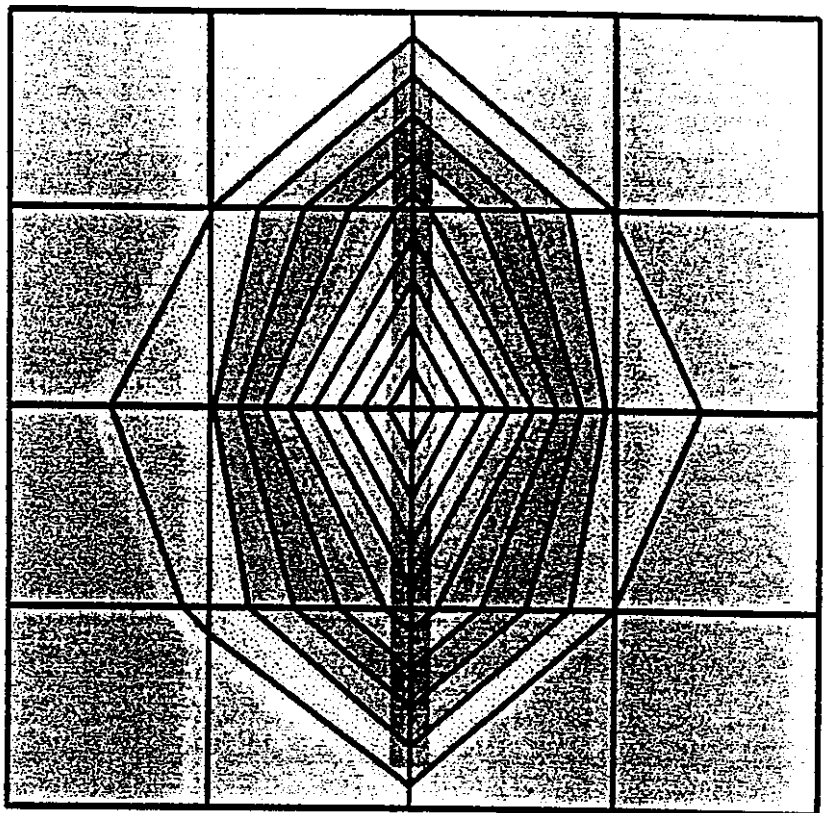
The dipole is made of standard semirigid coaxial cable. The centre conductor of the feeding line is directly connected to the second arm of the dipole. The antenna is therefore short-circuited for DC-signals.

Do not apply excessive force to the dipole arms, because they might bend. If the dipole arms have to be bent back, take care to release stress to the soldered connections near the feedpoint; they might come off.

After prolonged use with 40W radiated power, only a slight warming of the dipole near the feedpoint can be measured.

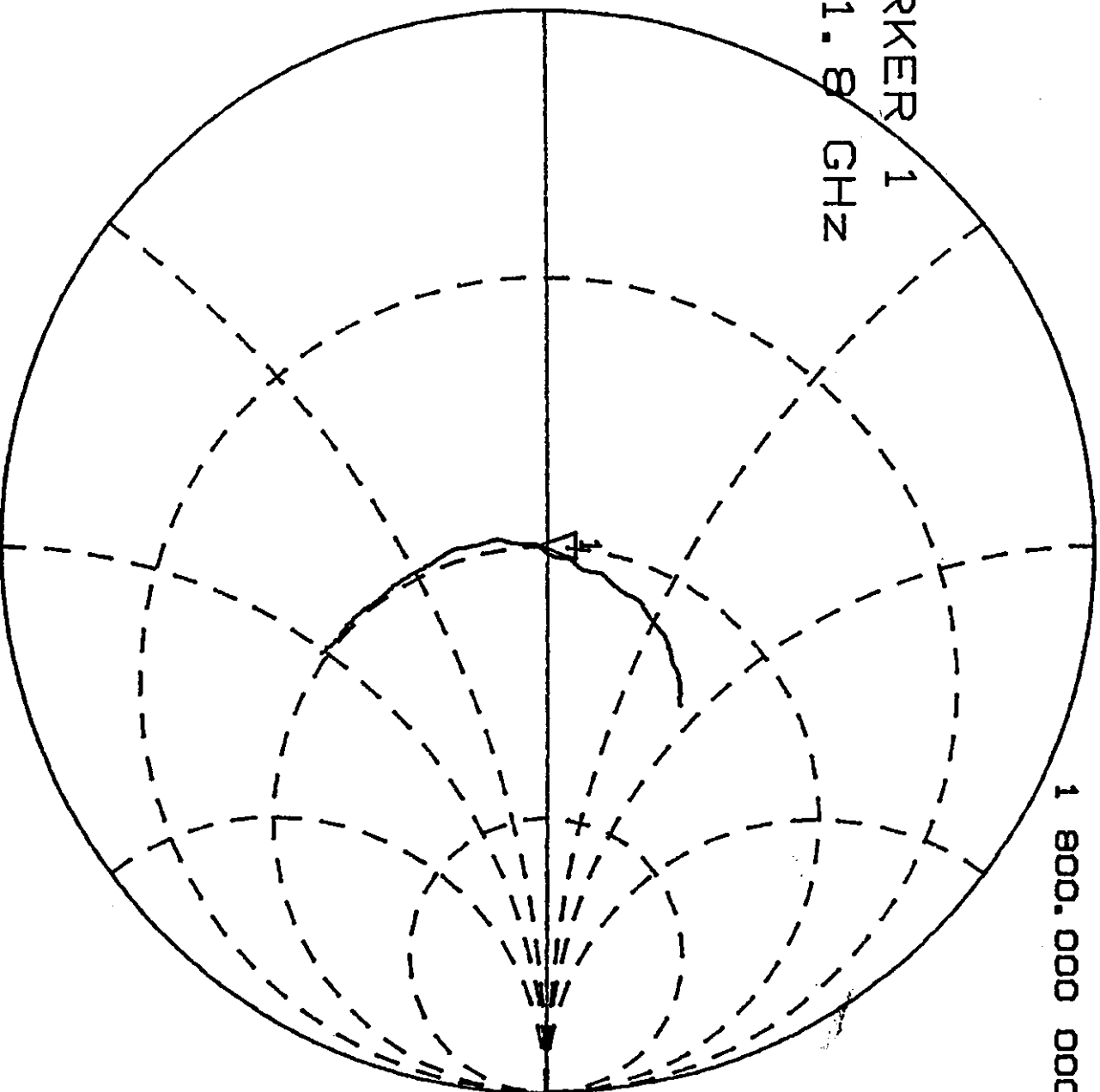
tion Dipole D1800V2 SN:207, d = 10mm

1800 [MHz]; Antenna Input Power: 250 [mW]
 win Phantom; Flat Section; Grid Spacing: Dx = 20.0, Dy = 20.0, Dz = 10.0
 3DV5 - SN1302/DAE3; ConvF(4.60,4.60,4.60); Brain 1800 MHz: $\sigma = 1.65$ [mho/m] $\epsilon_r = 40.1$ $\rho = 1.00$ [g/cm³]
 Peak: 18.1 [mW/g] ± 0.02 dB, SAR (1g): 9.27 [mW/g] ± 0.03 dB, SAR (10g): 4.63 [mW/g] ± 0.04 dB, (Worst-case extrapolation)
 n depth: 7.2 (7.0, 7.8) [mm]



1 S11	1 U FS	49.887	-1.4648	60.361	Pf
1 800.000	000	MHz			

1 MARKER 1
1.8 GHz

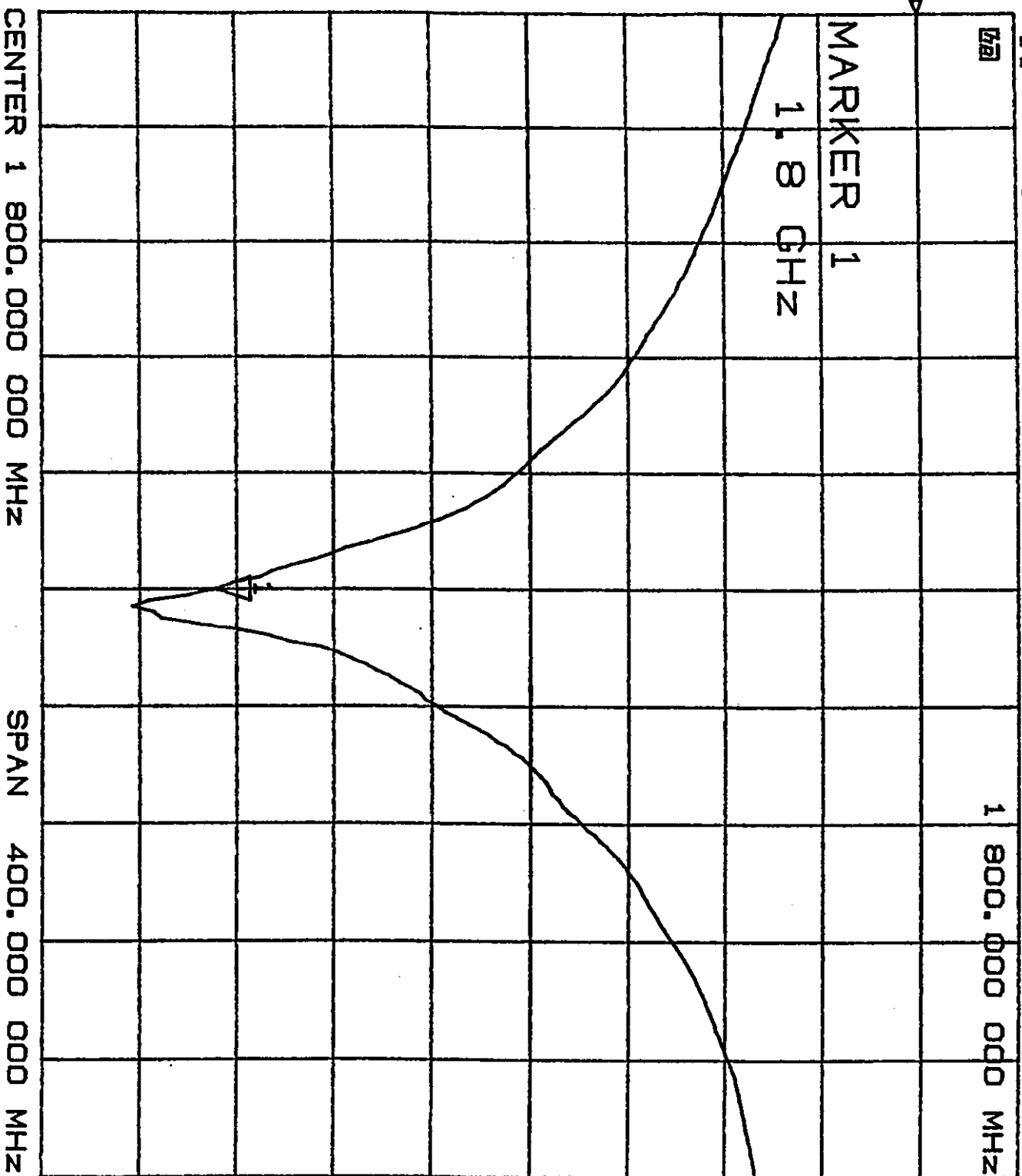


CENTER 1 800.000 000 MHZ

SPAN 400.000 000 MHZ

11 S11 log MAG 5 dB/ REF 0 dB 1 800.000 000 MHz 11-36.004 dB

MARKER 1
1.8 GHz



Appendix 9

page 1

VERIFY WITH DIPOLE VALIDATION KIT

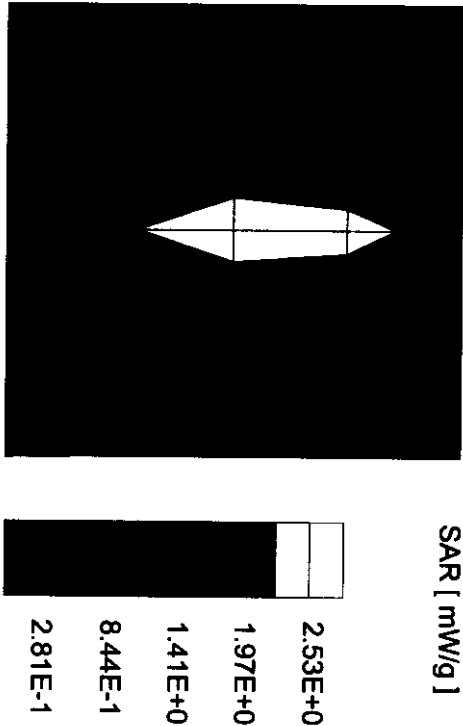
Verify with Validation Kit (D900V2 SN:003) / Generic Flat Phantom / f=900MHz/ Pin=250mW / d=15mm / 1998-Dec-17/NMP

$\sigma = 0.86$ [mho/m] $\epsilon_r = 41.3$ $\rho = 1.00$ [g/cm³]

Coarse Grid Dx = 15.0 Dy = 15.0 Dz = 5.0 [mm]

SAR [mW/g] Max: 2.53

SAR (1g): 2.38 [mW/g] SAR (10g): 1.53 [mW/g]



Appendix 10

pages 1 - 4

SAR MEASUREMENT RESULTS

THE APPLICANT'S represent-
ative CONFIRMS THAT THE
P.O. MEASUREMENTS SHOWN ON
S.A.R. RESULTS ARE

CONDUCTED MEASUREMENTS

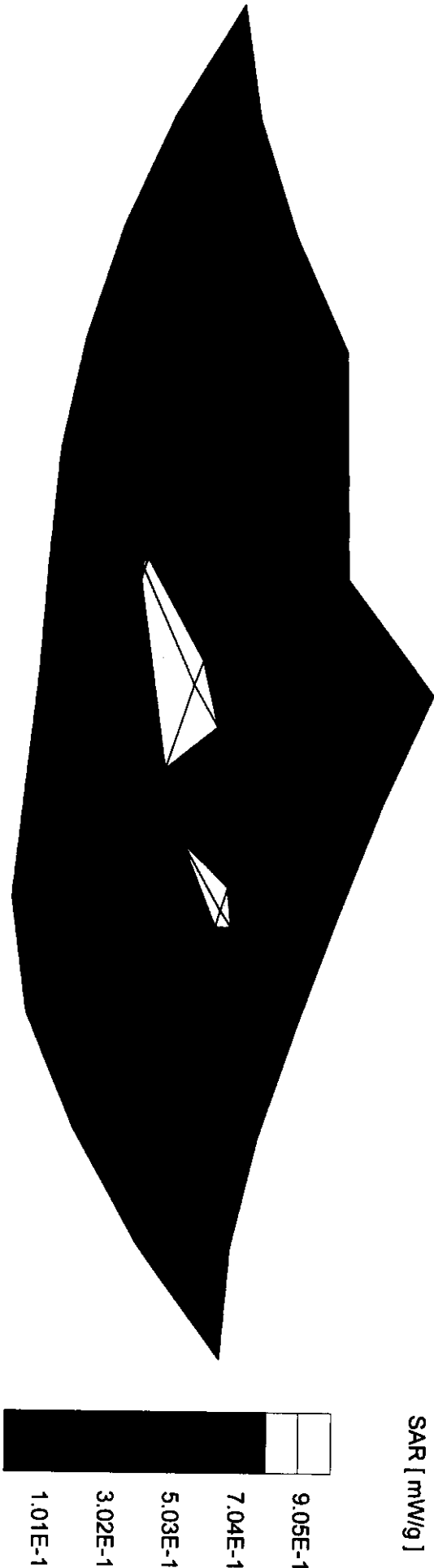
Nr:1, Type: NSD-1GX, (SN:32204), Channel 991, Po: +25.1dBm, Phone position 90deg, Measured: 17-Dec-1998/NMP, File: HD981C2.MEA

$\sigma = 0.79$ [rho/m] $\epsilon_r = 42.1$ $\rho = 1.00$ [g/cm³]

Coarse Grid Dx = 20.0 Dy = 20.0 Dz = 5.0 [mm]

SAR [mW/g] Max: 0.91

SAR (1g): 0.916 [mW/g] SAR (10g): 0.648 [mW/g]



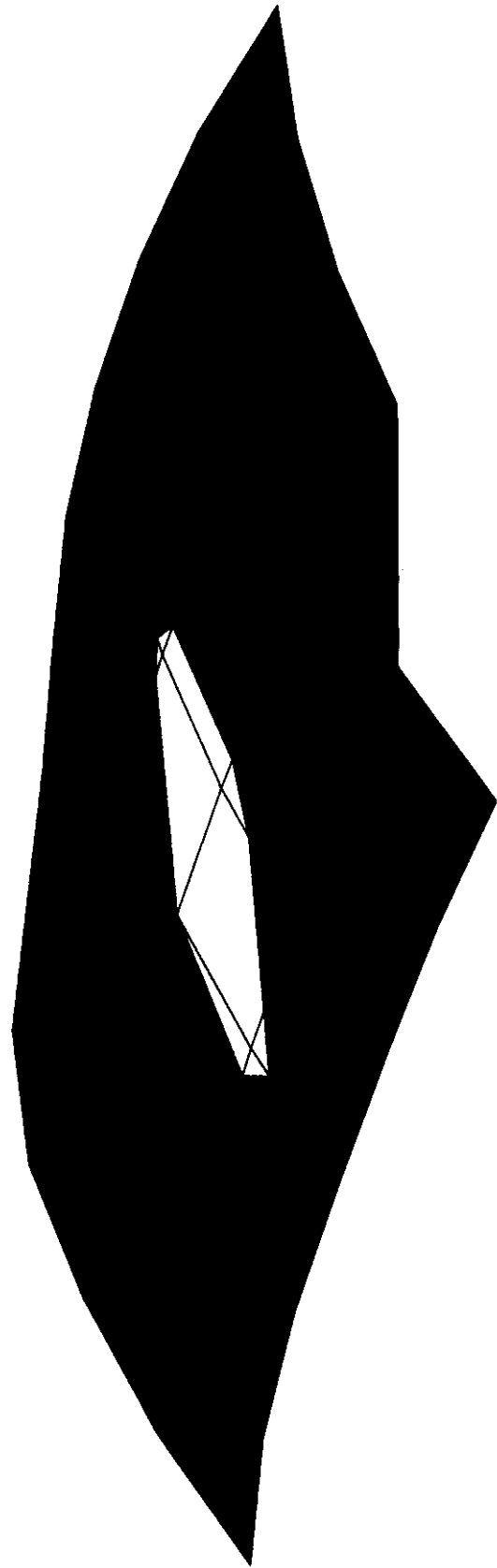
Nr:2, Type: NSD-1GX, (SN:32204), Channel 383, Po: +25.2dBm, Phone position 90deg, Measured: 17-Dec-1998/NMP, File: HD981C1.MEA

$\sigma = 0.80$ [mho/m] $\epsilon_r = 41.9$ $\rho = 1.00$ [g/cm³]

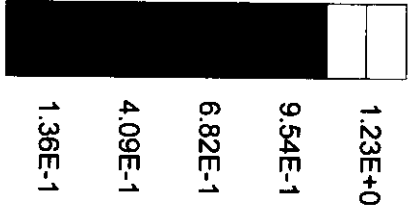
Coarse Grid Dx = 20.0 Dy = 20.0 Dz = 5.0 [mm]

SAR [mW/g] Max: 1.23

SAR (1g): 1.28 [mW/g] SAR (10g): 0.899 [mW/g]



SAR [mW/g]



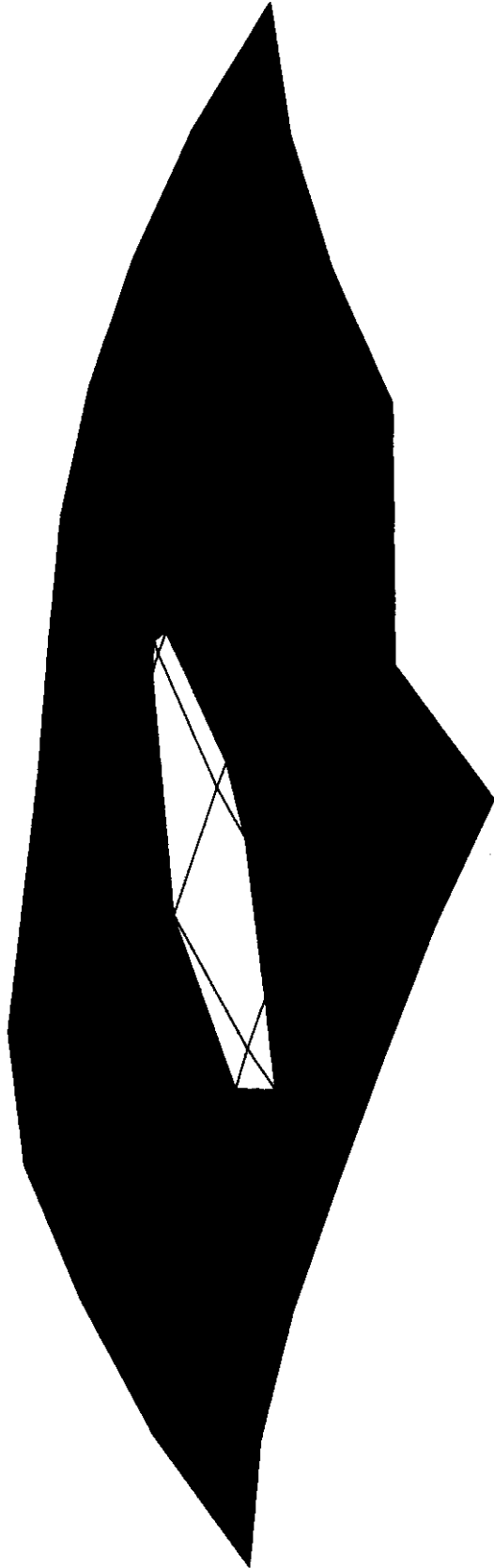
Nr:3, Type: NSD-1GX, (SN:32204), Channel 799, Po: +25.5dBm, Phone position 90deg, Measured: 17-Dec-1998/NMP, File: HD981C3.MEA

$\sigma = 0.81$ [mho/m] $\epsilon_r = 41.8$ $\rho = 1.00$ [g/cm³]

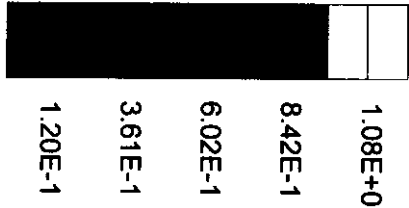
Coarse Grid Dx = 20.0 Dy = 20.0 Dz = 5.0 [mm]

SAR [mW/g] Max: 1.08

SAR (1g): 1.09 [mW/g] SAR (10g): 0.777 [mW/g]



SAR [mW/g]



Nr.2, Type: NSD-1GX, (SN:32204), Channel 383, Po: +25.2dBm, Phone position 90deg, Measured: 17-Dec-1998/NMP, File: HD981C1.MEA

$\sigma = 0.80$ [mho/m] $\epsilon_r = 41.9$ $\rho = 1.00$ [g/cm³]

Coarse Grid Dx = 20.0 Dy = 20.0 Dz = 5.0 [mm]

SAR [mW/g] Max: 1.23

SAR (1g): 1.28 [mW/g] SAR (10g): 0.899 [mW/g]

